

How does the brain work?

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UM Hemisphere Institute



Table of Contents



■ 1) We know

- Anatomy
- Electrical Activity
- Bio chemistry

■ 2) Goals of theoretical Neuroscience

- Identify Areas responsible for different functions
- Brain Mechanism vs behavior/cognition/emotions
- To understand how does the brain works?

■ 3) My Targets

- Synchronization and compositionality
- Numeration in the Brain
- From Neuro to Finance
- Ethics of Brain Machine Interface
- Bio-medical Projects (Sleep disorder and Epilepsy)

We know

ANATOMY

- Different sections of the brain
- 10^{10} neurons
- Axon and dendrites
- Dendrites travel far
- White stuff
- Some localization of functions

ELECTRICAL ACTIVITY

- Synapses

BIOCHEMISTRY

- Neurotransmitters (Biochemistry)

We DON'T know:

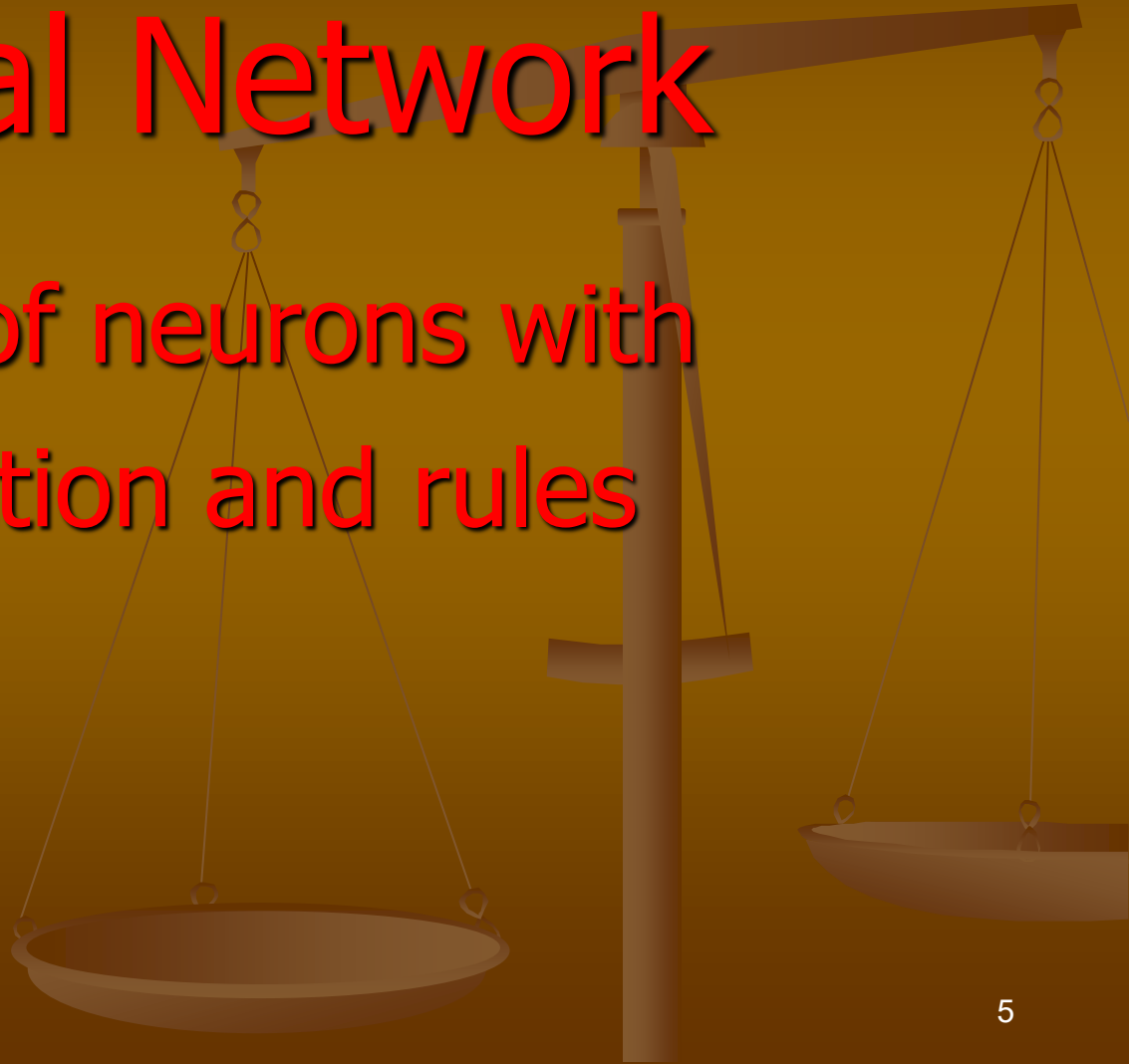
- Precise location of cognitive/emotional functions
- Cognitive and emotional functions representation in the brain
 - Language mechanisms
 - Numeration representations
 - Mathematical skills
 - Musical skills
- How does the network works as a whole ?
 - Which neuron “speaks” to which neuron?
 - What are the rules?
 - How to handle huge (!) amount of data

....

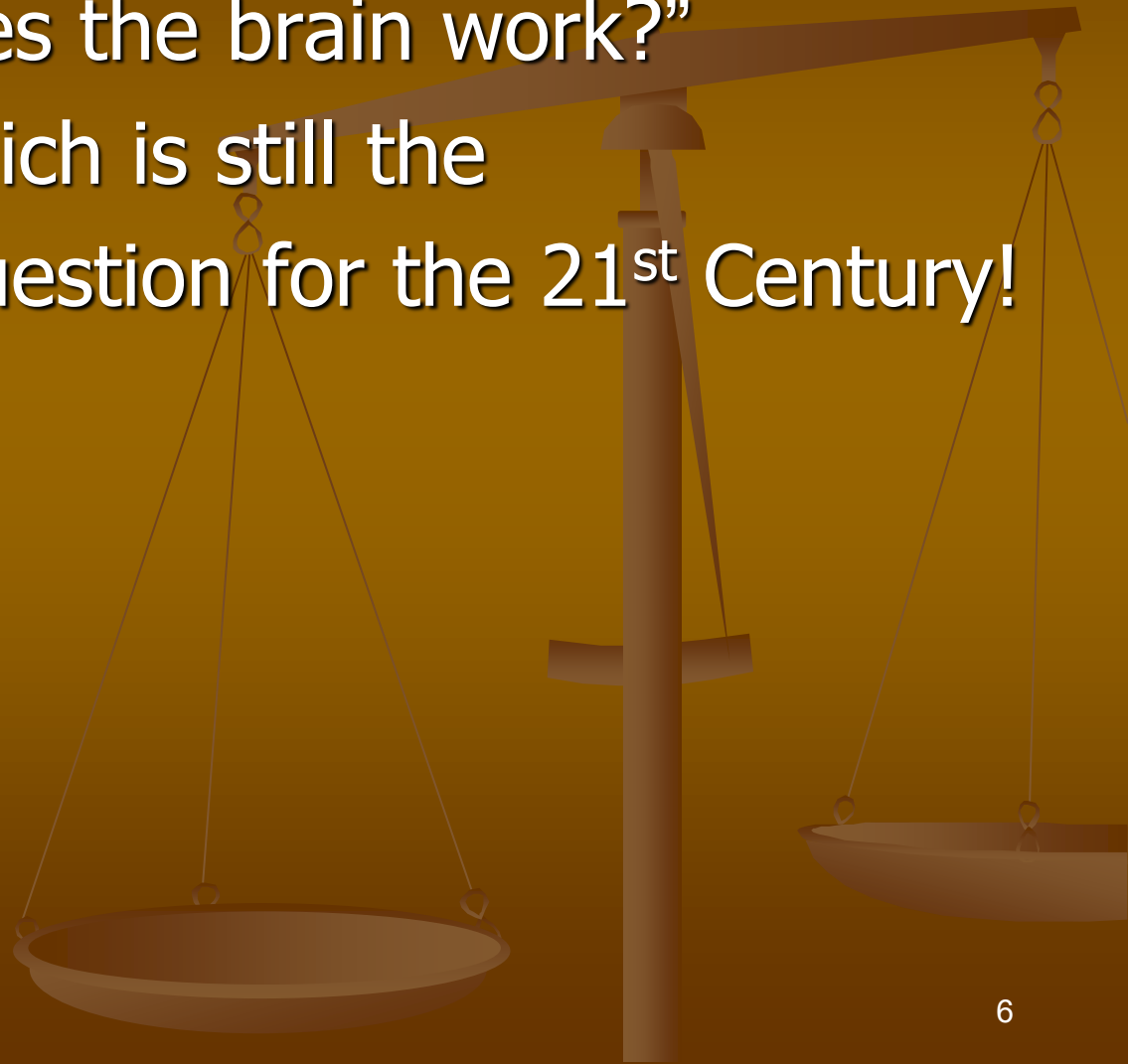
Trying to understand how does the brain works we localize the problem to

Neural Network

= a set of neurons with
an action and rules

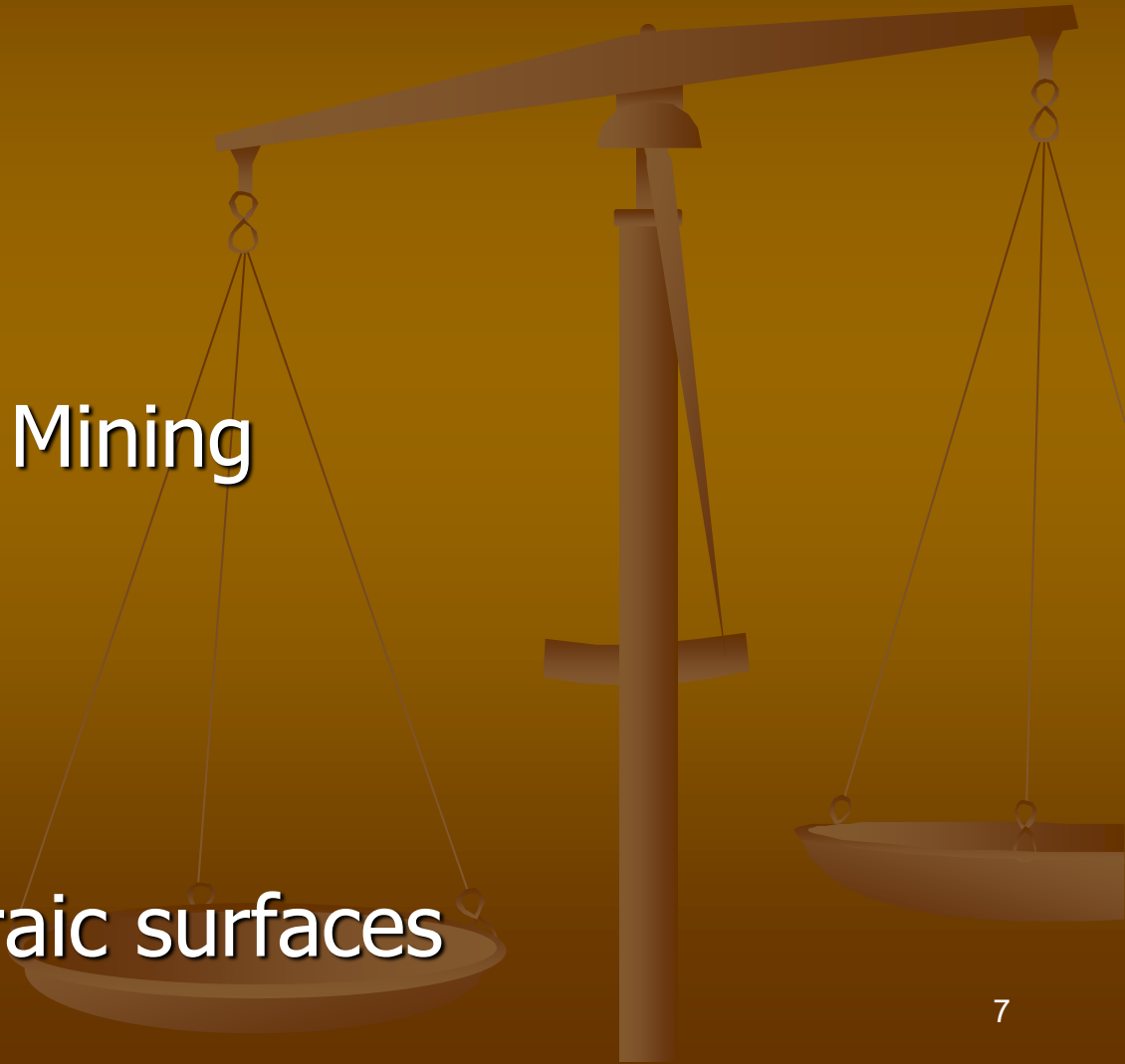


“How does the brain work?”
which is still the
most intriguing question for the 21st Century!



Mathematical Methods from

- Dynamical systems
- Stochastics
- Wavelets
- Singularities
- Geometric Data Mining
- Statistics
- Probability
- Moduli of algebraic surfaces



We start with Brain Imaging

Imaging =
Recording device
plus a
Forgetful functor
plus a
Cleaning mechanism



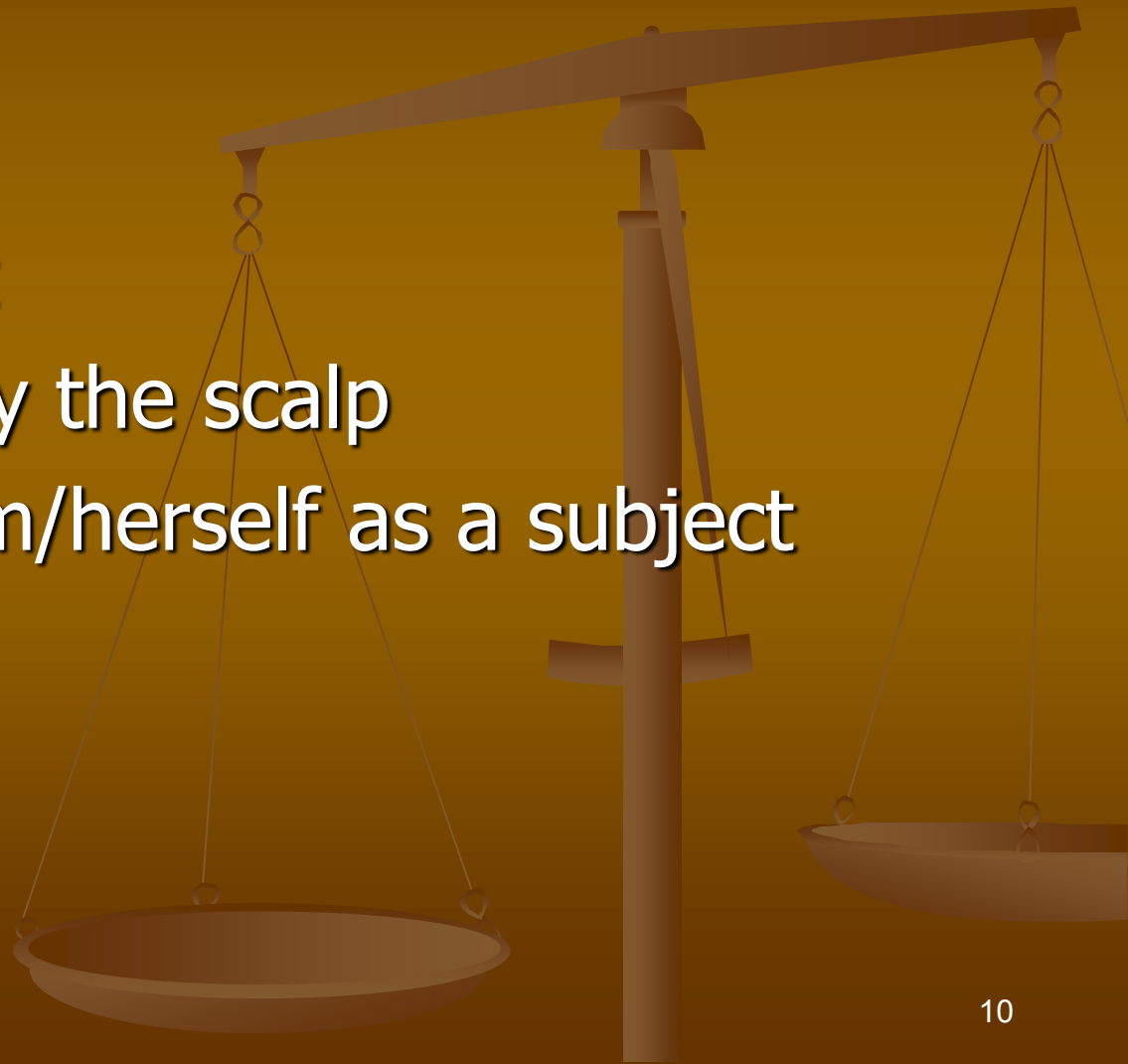
Imaging Techniques

- Inter cellular recording
- EEG
- MEG
- PET SCAN
- fMRI



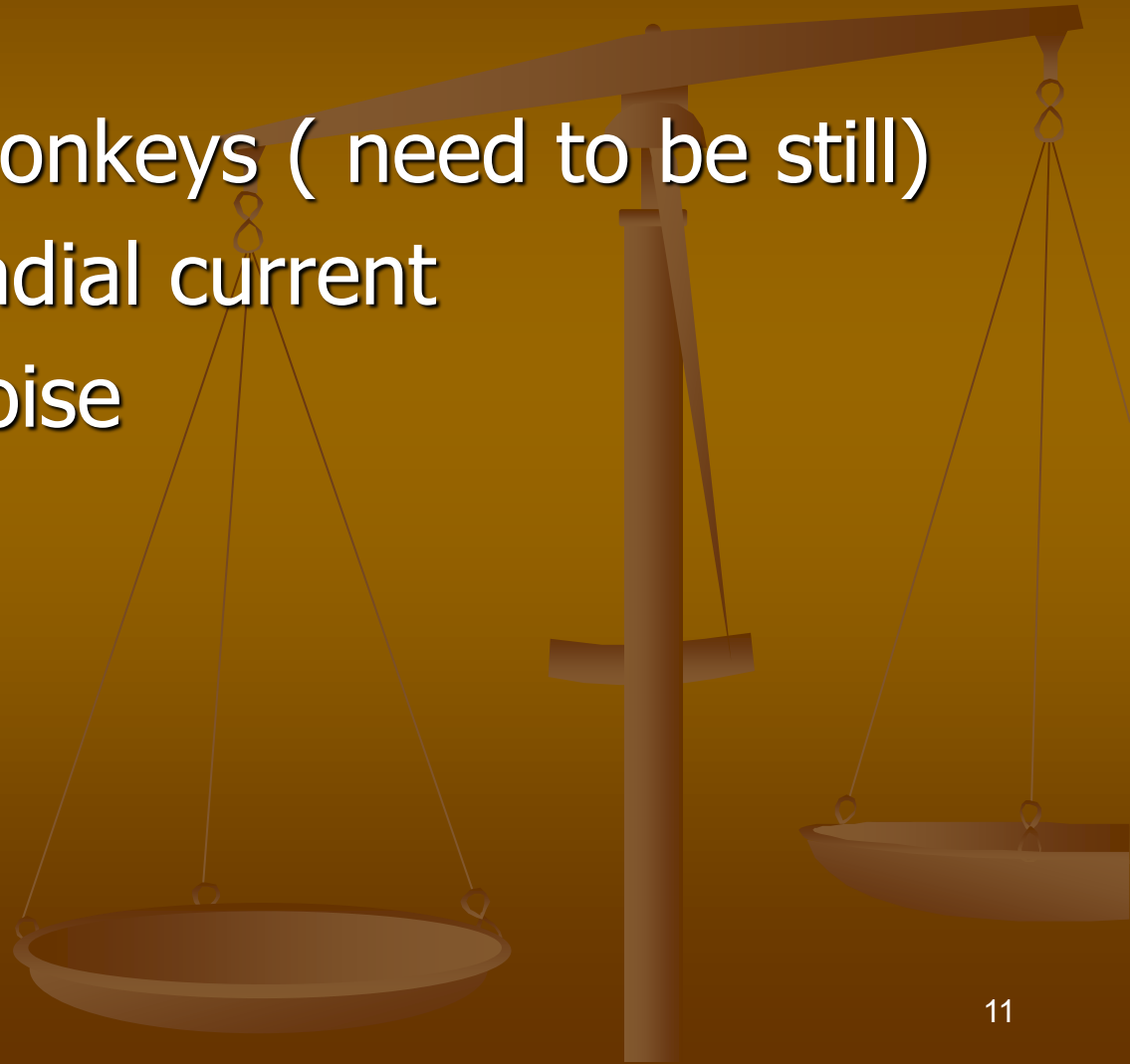
Advantages of MEG over EEG

- No touch
- 248 channels
- Easy to connect
- Not disturbed by the scalp
- One can use him/herself as a subject



Disadvantages

- No touch
- One cant use monkeys (need to be still)
- Not detecting radial current
- Low signal to noise
- 3MEuro



BIU MEG

- 248 Magnetometewholehead MEG system (WH3600, 4D)
- Simultaneous EEG recording
- Eye tracking
- A complete set of stimulation systems
- The MEG is inside a double wall magnetically shielded room by IMEDCO
- Cleaning and maintenance by Moshe Abeles/Squids, ect

What imaging devices do I use?

THEORY

SINCRONIZATION:

Inter Cellular recording on primates

Musical skills, Numeration, mathematical skills, metaphors

MEG (and fMRI)

BIO-MEDICINE

Epilepsy: EEG, EEG under scalp

Sleep Disorder: EEG plus

ADHD in rats Inter Cellular recording

Students that contributed

Mina Teicher



יקי שטרן



לילך אביטן



אורי ירושלמי



יקיר ברצ'נקו



אמיר קלקס



תומר גזית



יואל פנחס



אורן שמיאל



ענבל לוטוס

A.

First proof of

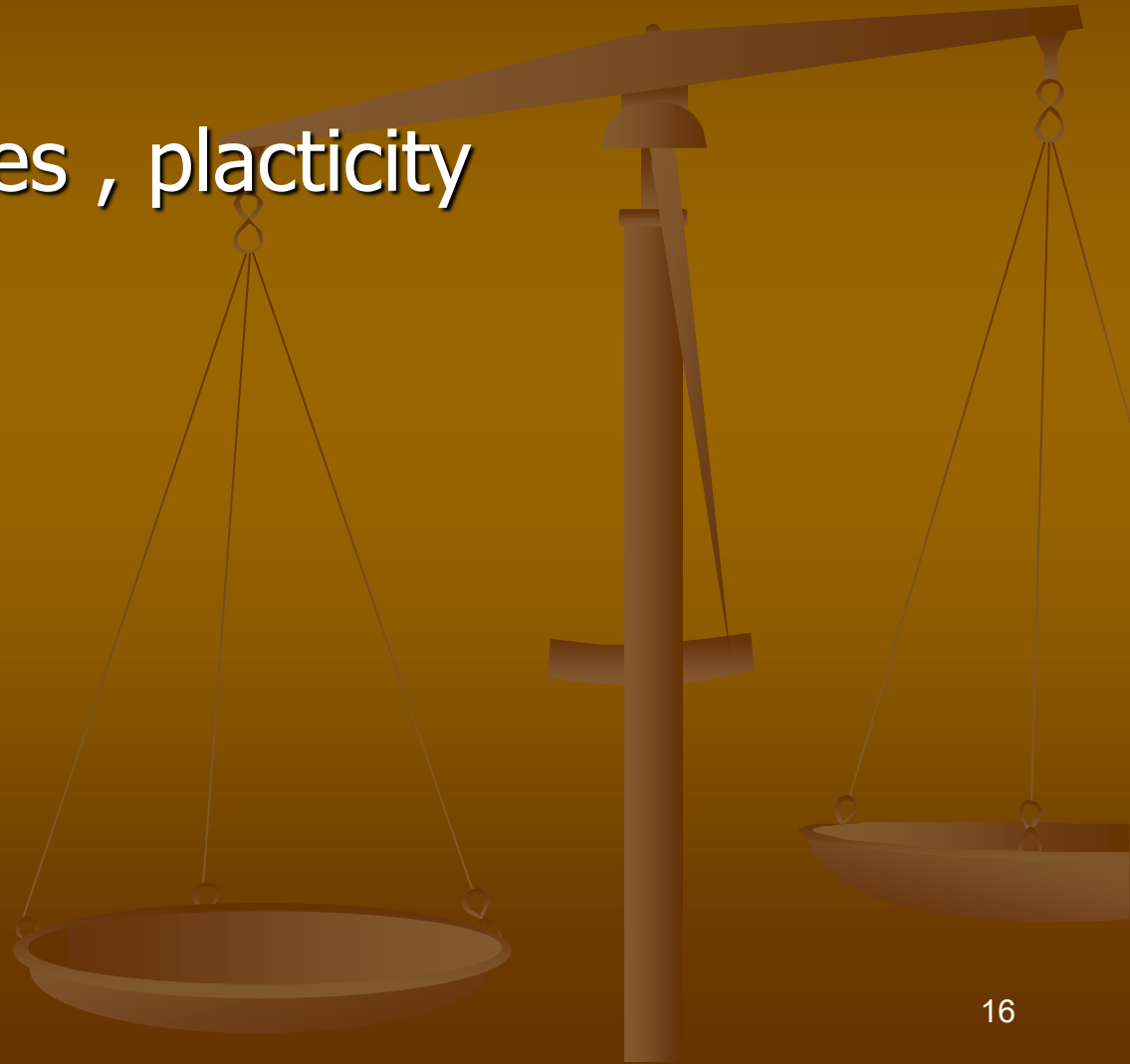
Synchronization

in behaving animals



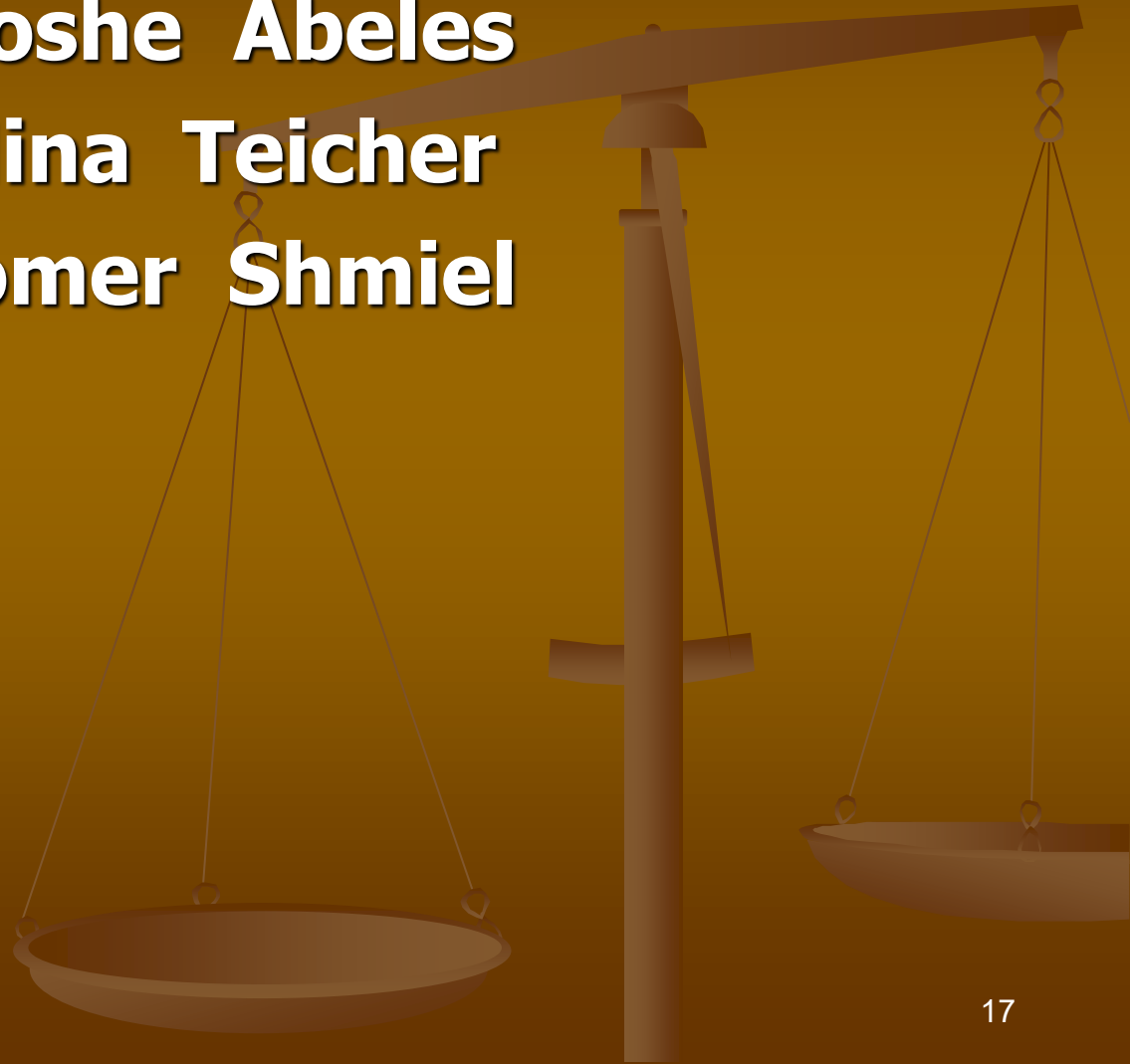
Conjectures on the way the Brain activity works

- Chaos , firing rates , placticity
- Synchronization
- Compoisionality
- Synfire Chains



Spikes Synchronization and Hand Motion

- **Moshe Abeles**
- **Mina Teicher**
- **Tomer Shmiel**



Goals

Finding (unknown) relationships between hand-motion and brain-activity which are **NOT** induced from the population vector (frequency and direction ($\sum f_i v_i$))

We will focus on accurate spike patterns using computerized methods

The Experiment:

Sampling Monkey's Drawings

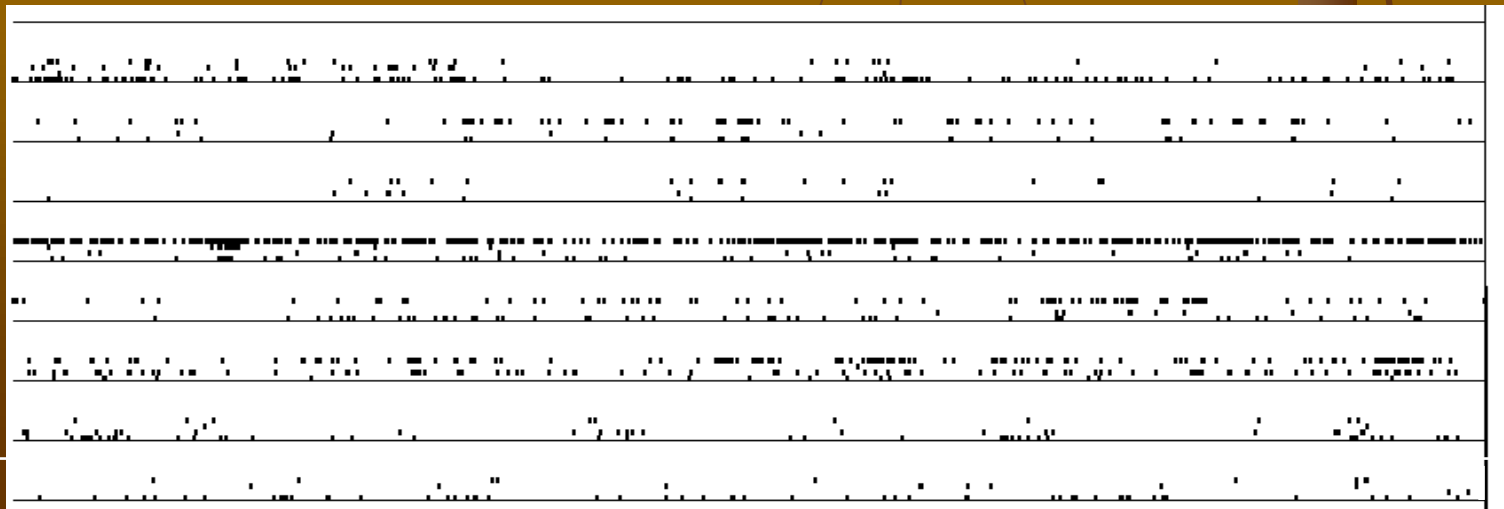
Drawings by manipulandum are sampled at 100Hz



The Experiment:

Recording Neural Activity

- Recording brain activity using 8 micro-electrodes inserted under the scalp into the motor (and pre-motor) cortices
- Identifying stable individual neurons
- Spike-sorting for separating the electrical signals from each electrode to different neurons
- The data still contains spike noise



sec 20

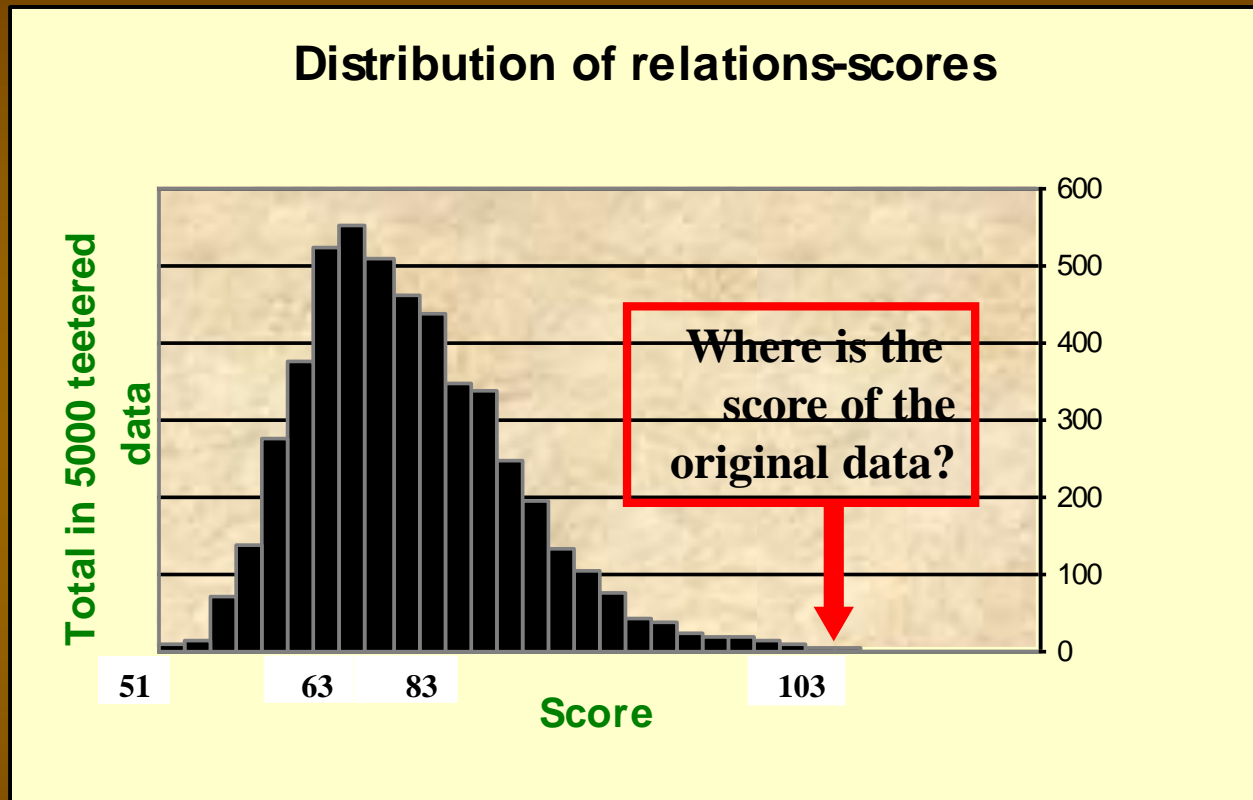
We are also interested in the **Strength of a Relationships**

To each experiment day we give a "score "
(in a numerical value) that gives an
estimate measure to the precise
correspondence (synchronization)
between activity and brain

This is done in 7 steps

Results

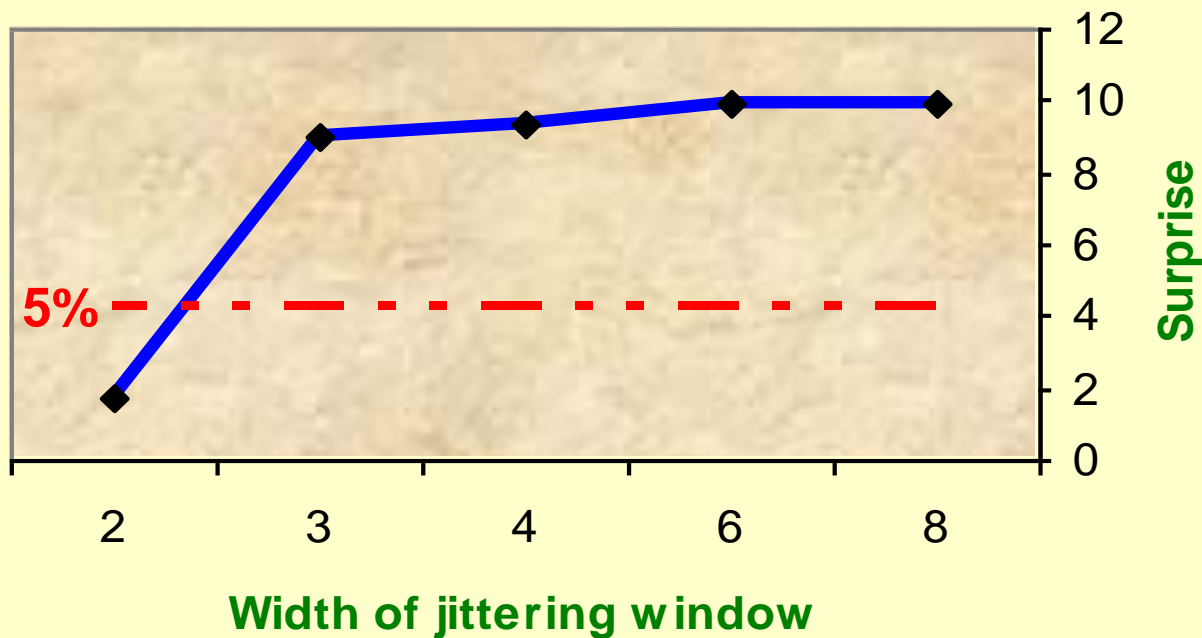
(jittering-window used: 10ms)



None of the 5000 jittered data has reached the original score!!!

Results (cont.)

Surprise vs jittering window



Significance of 0.2% for jittering window=3ms

Conclusions

Spikes hold information in a time resolution of 3 milli-seconds

This information seems to be related to the hand-motion direction and velocity

B. Numeration

Work in Progress

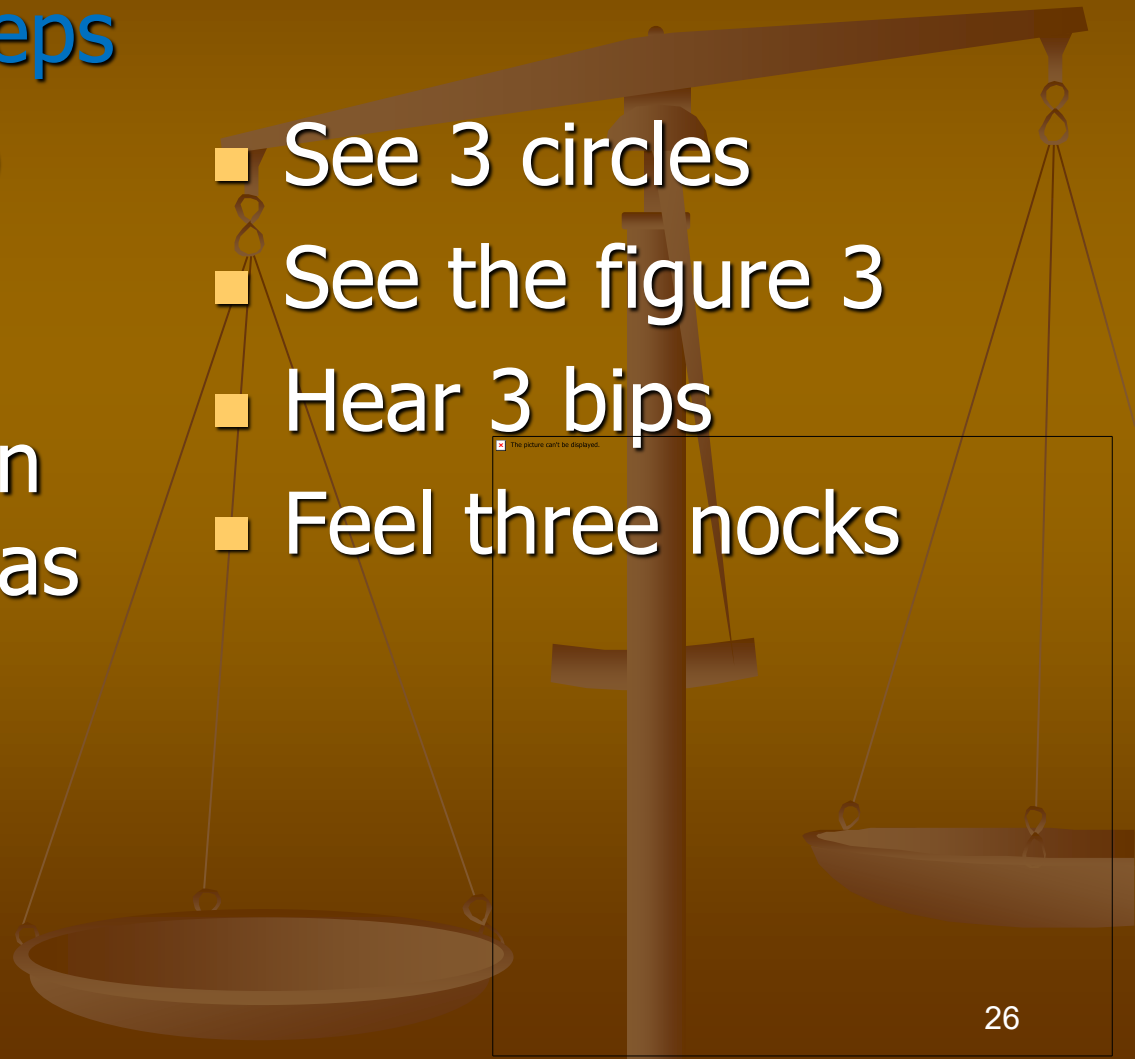
Ahmad Sleman
Amir Kleks
Yael Eisenberg
Mina Teicher



Is there a concept of a number in the brain?

Initial steps

- Via **MEG** We try to find a common phenomena or a common location in the brain for no 3 as reaction to
 - See 3 circles
 - See the figure 3
 - Hear 3 bips
 - Feel three nocks



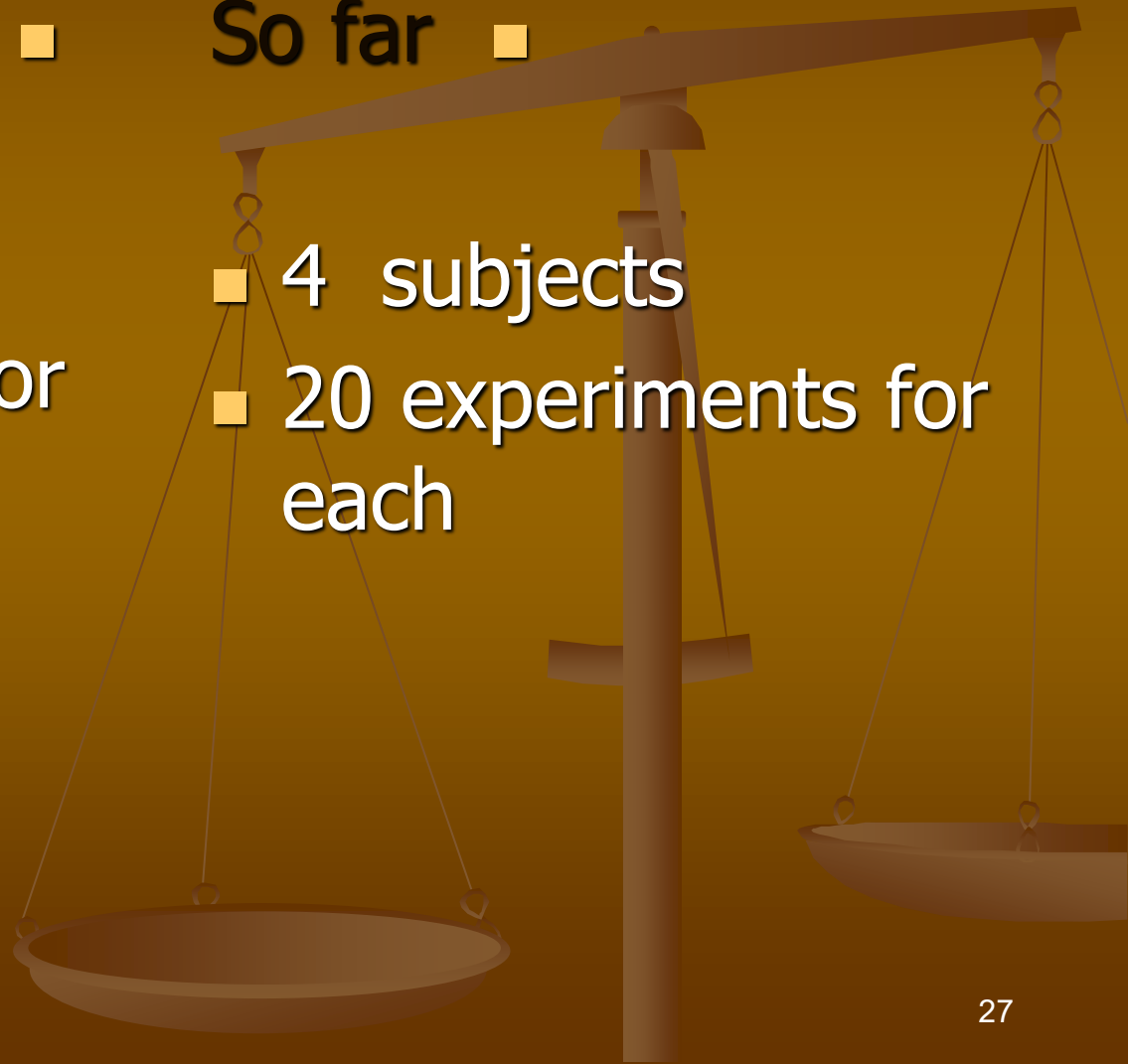
Is there a concept of a number in the brain?

Plan to record MEG data from

- 20 subjects
- 100 experiments for each

So far

- 4 subjects
- 20 experiments for each



Is there a concept of a number in the brain?

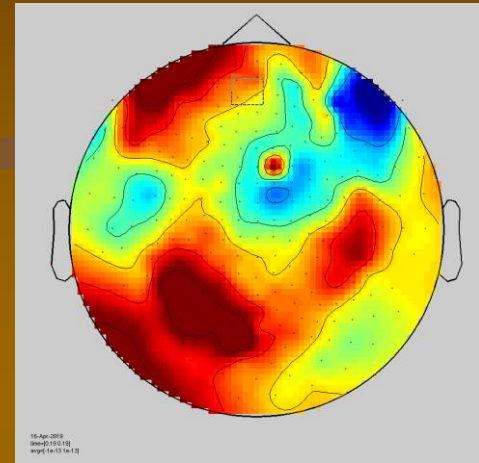
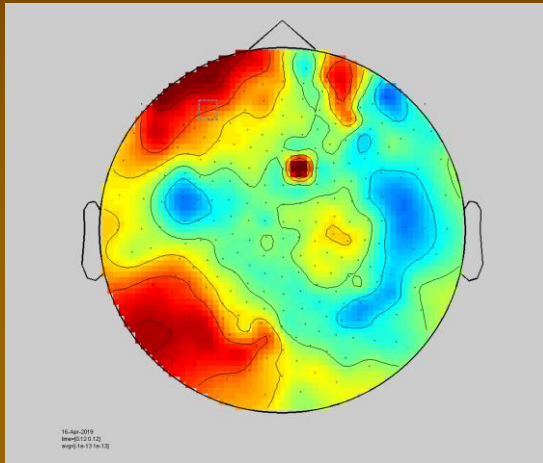
Plan to use on 4D MEG
the recording :

- Cleaning
- Matlab
- SAMBeamforming
- Data Mining



BIU Method for cleaning

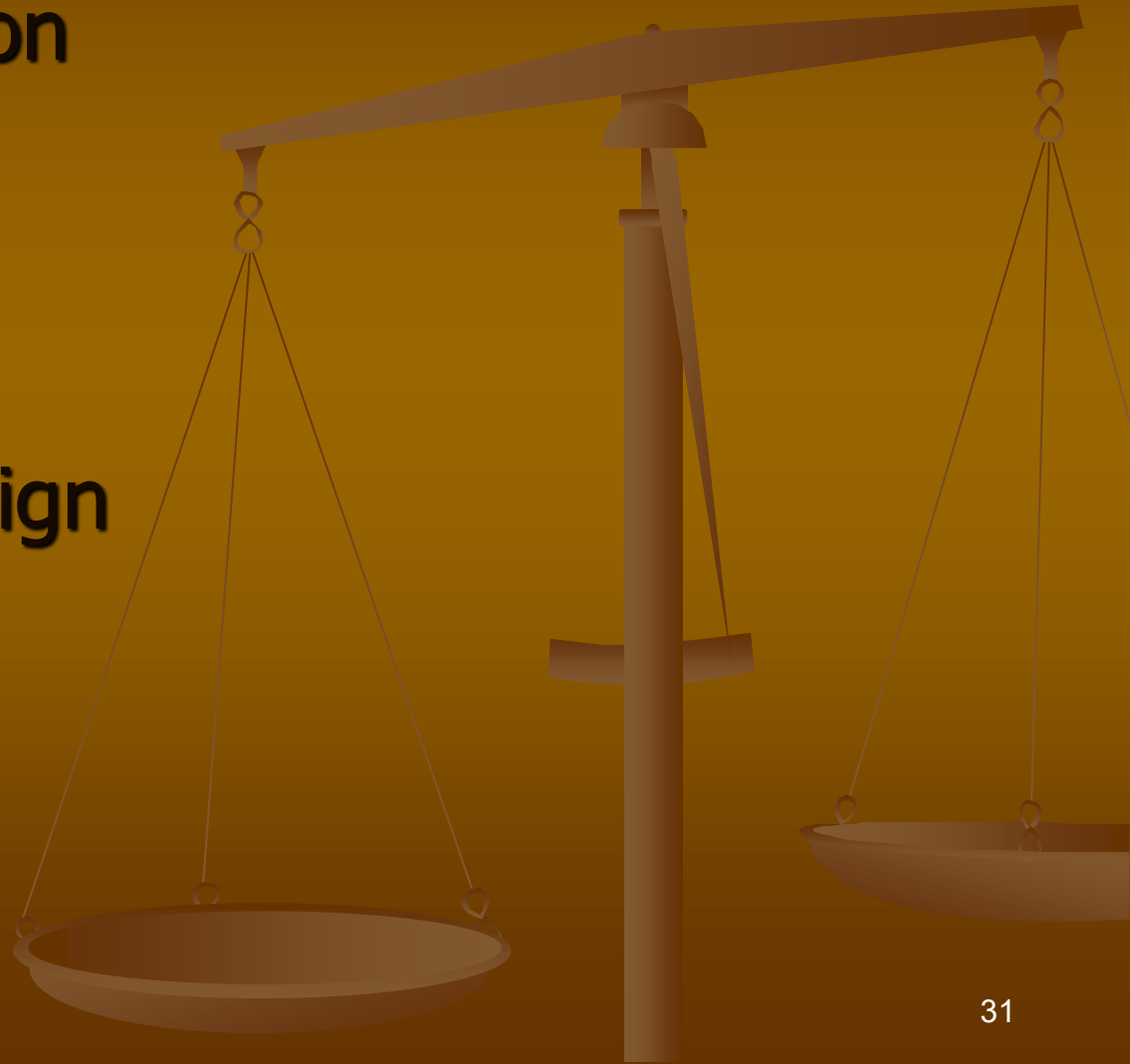
- Cleans the data of 50Hz+ harmonics
based on line side recording
- Cleans the building vibrations
based on accelerometers recording
- Cleans the data
based on reference channels
- Applying different sets of weights
for different frequencies



Some open question in consultation with linguistic experts

1) is there a common
location for
THREE and THIRD?

2)What about 3 in Sign
Language ?



C. Ethics of Brain Machine interface



Work in Progress ■

Short version published in Nature letters ■
2018

D. MEDICAL PROJECTS

- Sleep Disorders

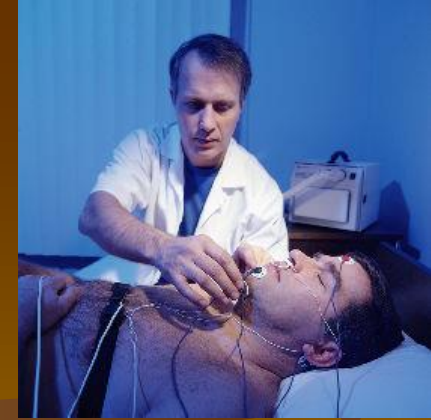


Recognition of Sleeping Phenomena

■
Prof. Yaron Dagan, Sleep Laboratory, TH Hospital and my PhD student Oren Shmiel

we produced a way ■
to predict sleep arousals
from synchronized channels

The Experiment:



Simultaneous measures of the following channels:

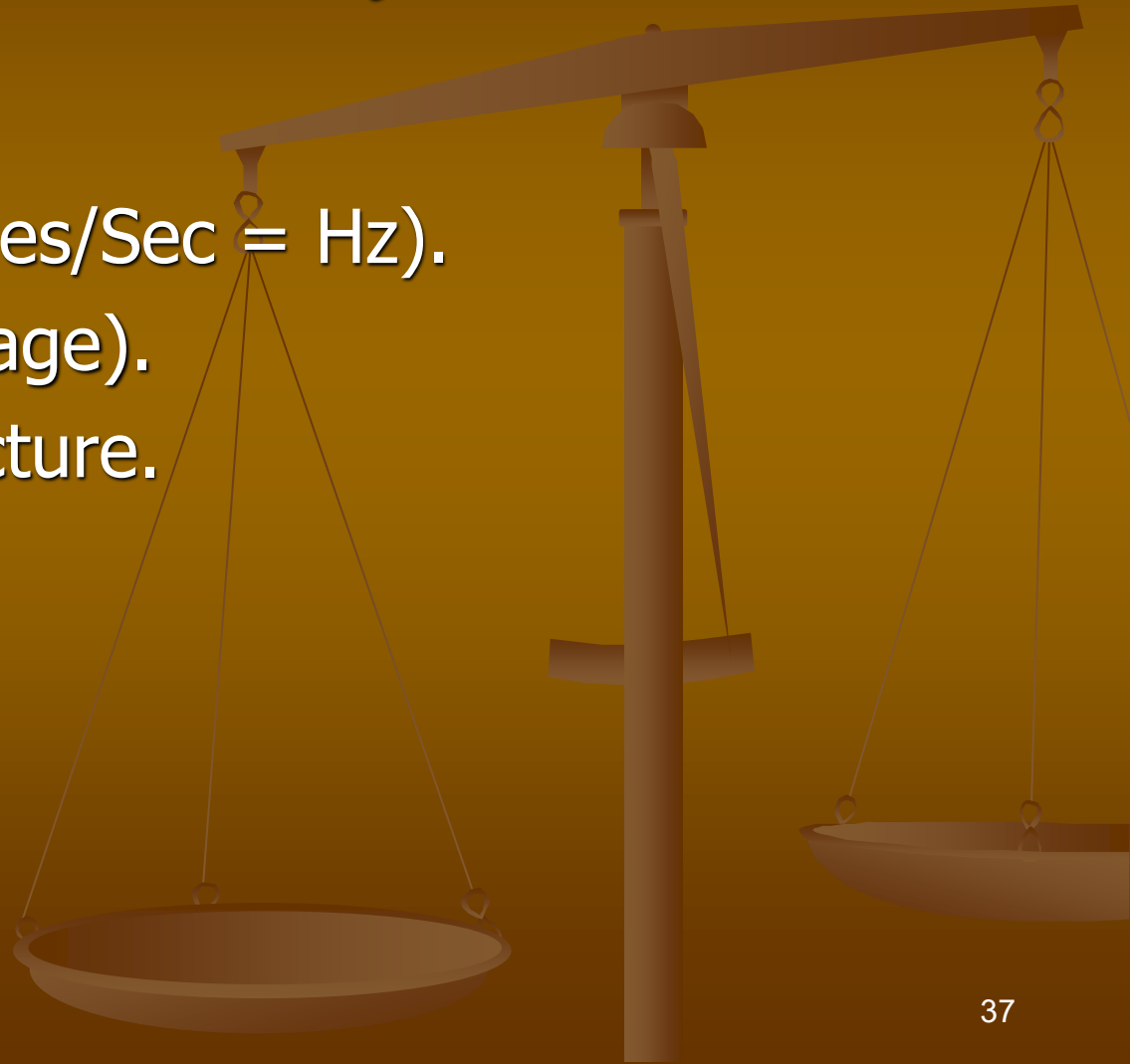
Channel	Description	Sampling (Hz)
EEG	מוח	100Hz
EOG	עיניים	100Hz
EKG	לב	200Hz
EMG Submental	שרירי סנטר	200Hz
EMG tibialis	שרירי רגליים	200Hz
Pulse	דופק	1Hz
SaO2	סטורציה (ריווי חמצן)	1Hz
Air Flow	נשימת אף	10Hz
Thorax, Abdomen	בטן וחזה	10Hz
GSR	מוליכות העור/הזעה	200Hz
Snore	נחירות	200Hz
Position	תנוחת גוף	35Hz

Goals

- 1) Prediction of **pre-sleeping behavior** from channels which can be recorded easily
- 2) Prediction of **arousals** in channels which can be recorded easily.
- 3) Relationships between the **GSR and other channels** (especially EEG, EOG, EMG).

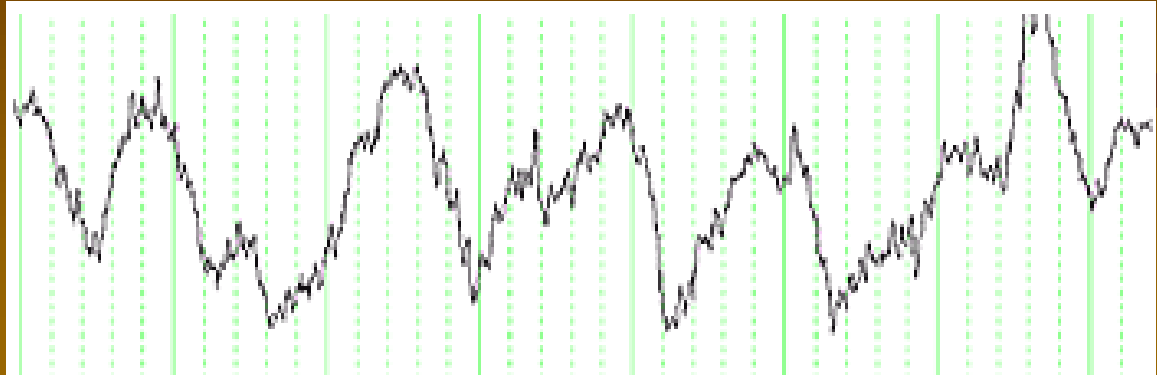
EEG Recordings in Sleep Research are classified by:

- Frequency (Cycles/Sec = Hz).
- Amplitude (Voltage).
- Shape and structure.

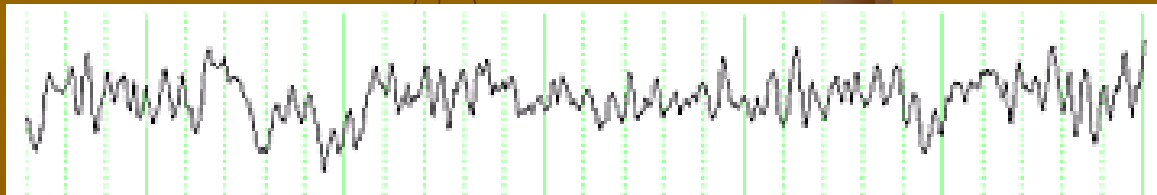


EEG Frequency in the different sleep phases

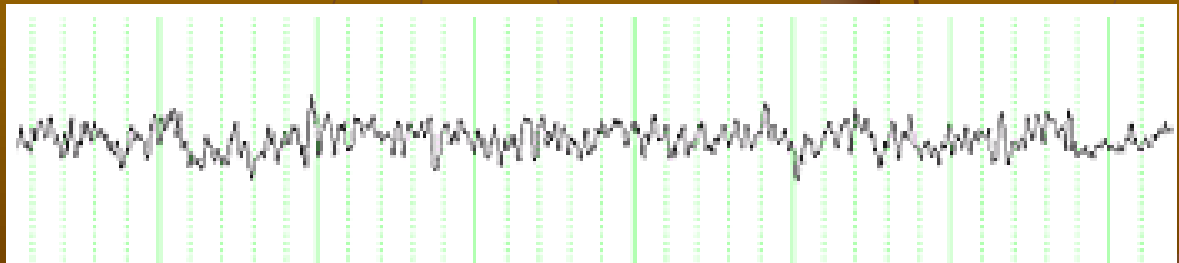
Delta (0-4 Hz)



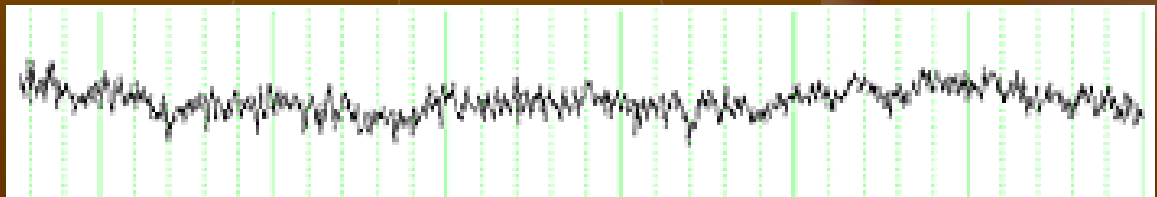
Theta (4-8 Hz)



Alpha (8-13 Hz)

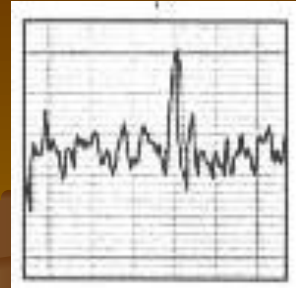


Beta (> 13 Hz)

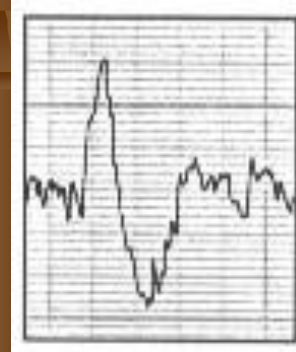


EEG Shape and structure

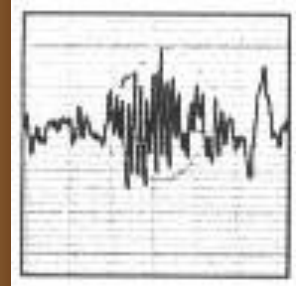
Vertex Waves: Sharp negative waves.



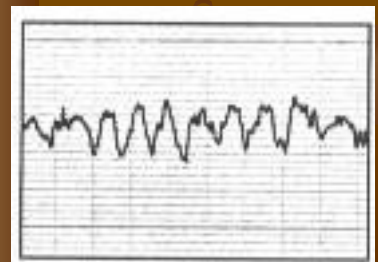
K-complex: A sharp negative wave followed by a slower positive component.



Sleep spindles: Short clusters of 12-14Hz.



Sawtooth waves: Low amplitude, saw tooth appearance.



Sleep Stages

Stage 1:

- Low amplitude mixed frequency in EEG.
- Vertex waves (at late part) in EEG.
- Slow eye movements in EOG.

Stage 2:

- Sleep spindles and K complexes in EEG.

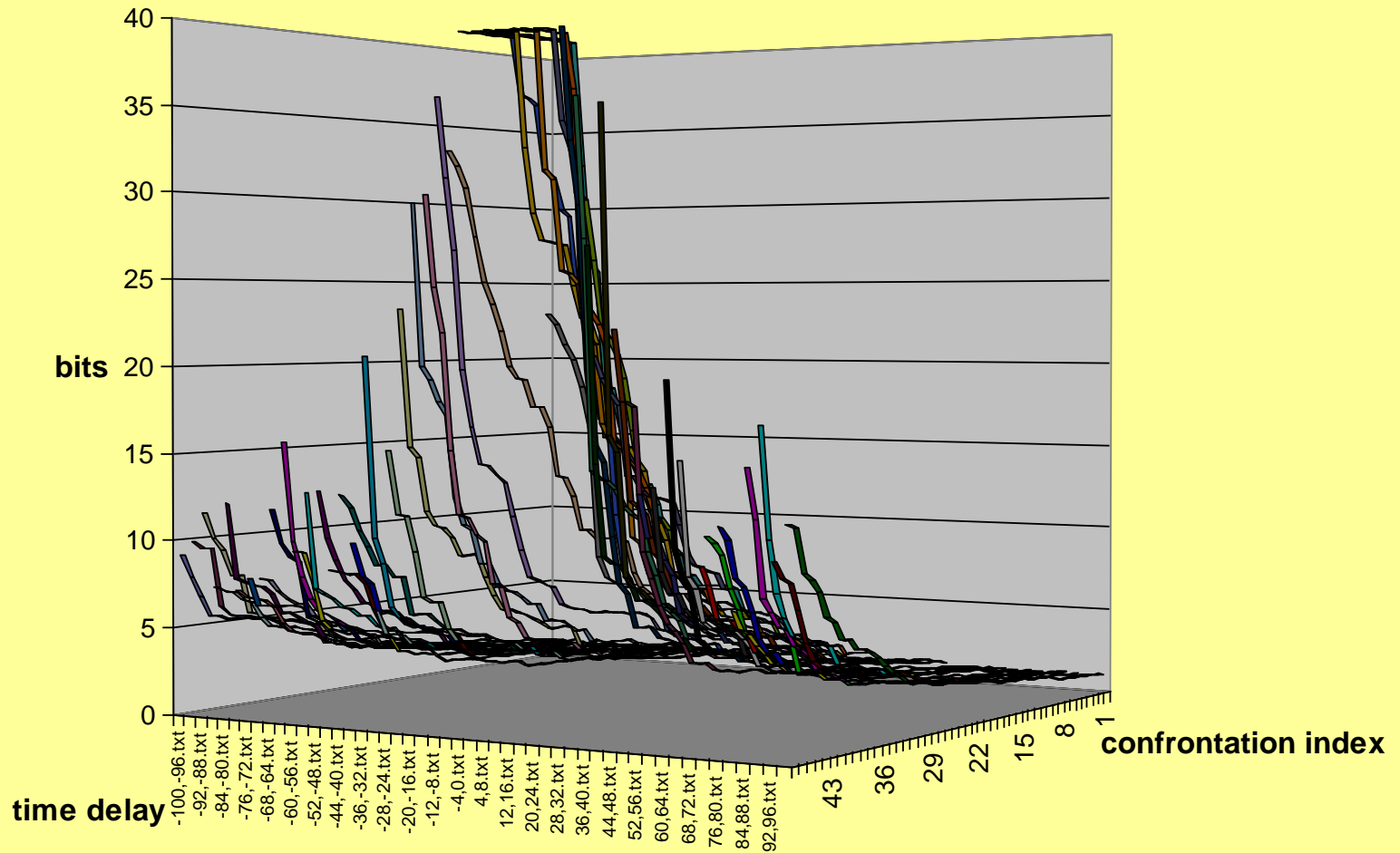
Stages 3,4:

- Delta waves with high amplitude in EEG.

Stage REM:

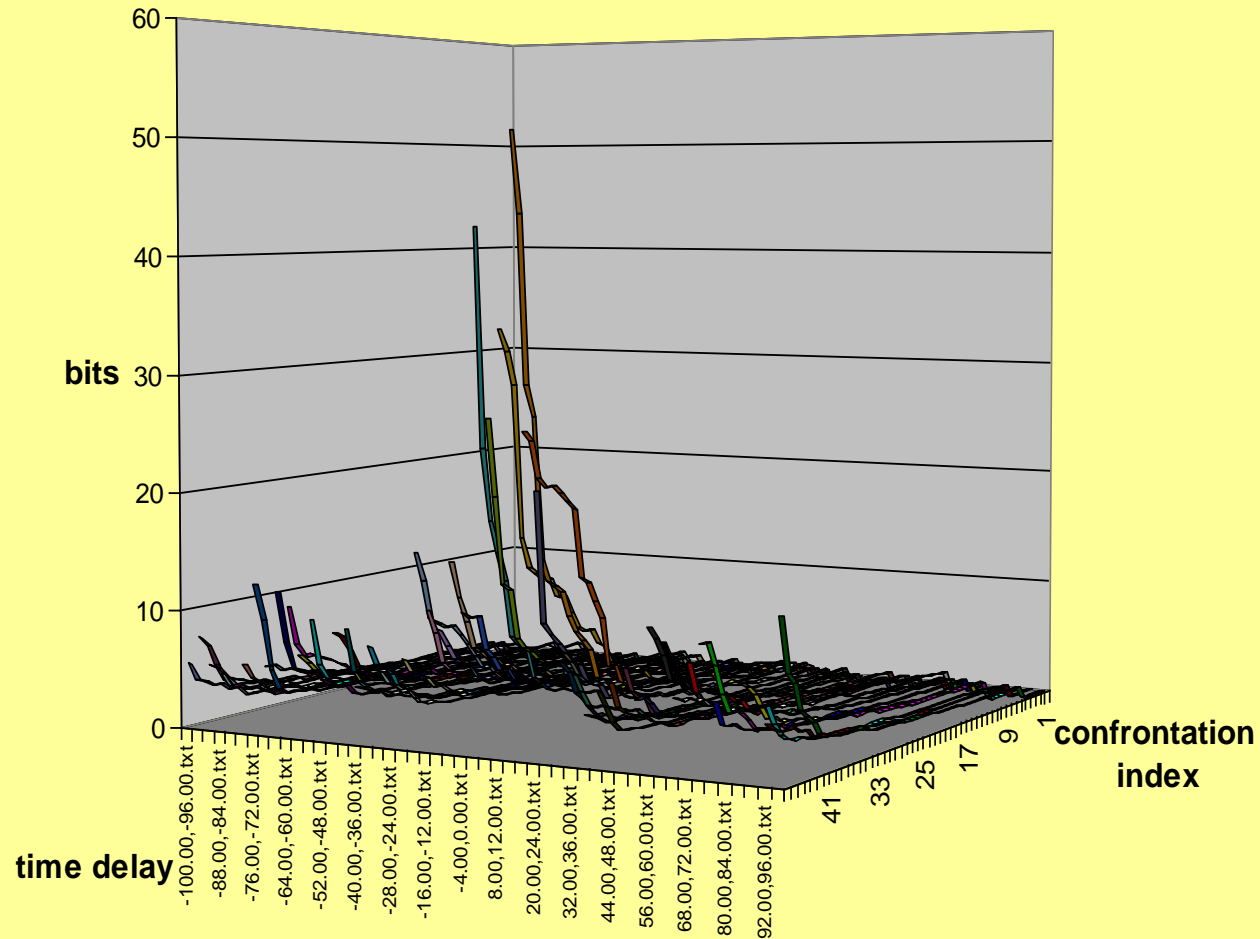
- Segments of Rapid Eye Movements in EOG.
- Low amplitude, mixed frequency in EEG.
- Saw tooth waves seen in many patients in EEG.
- Decrease in amplitude to the lowest level in EMG.

Preliminary RESULTS: Pulse vs SaO2



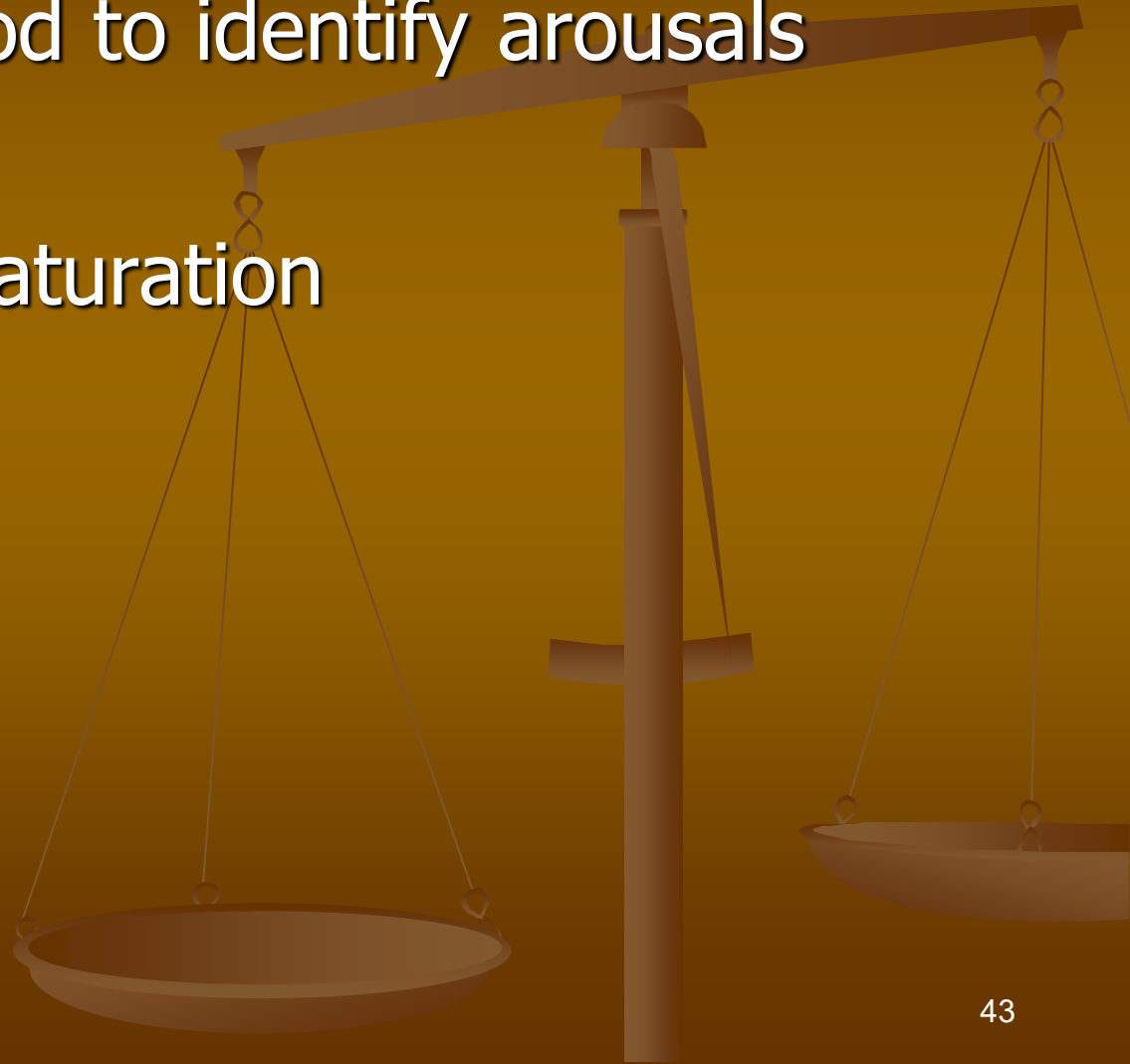
Preliminary RESULTS:

Pulse vs GSR



In Progress: : Detecting Arousals

Computerized method to identify arousals
from
EEG, EMG, Pulse, Saturation



E. From Neuro to Finance



We extend and ask what is the common to the below Examples

- a. Financial Markets
- b. The Brain
- c. Cities and Transportations
- d. Health Systems

They are all Complex System!

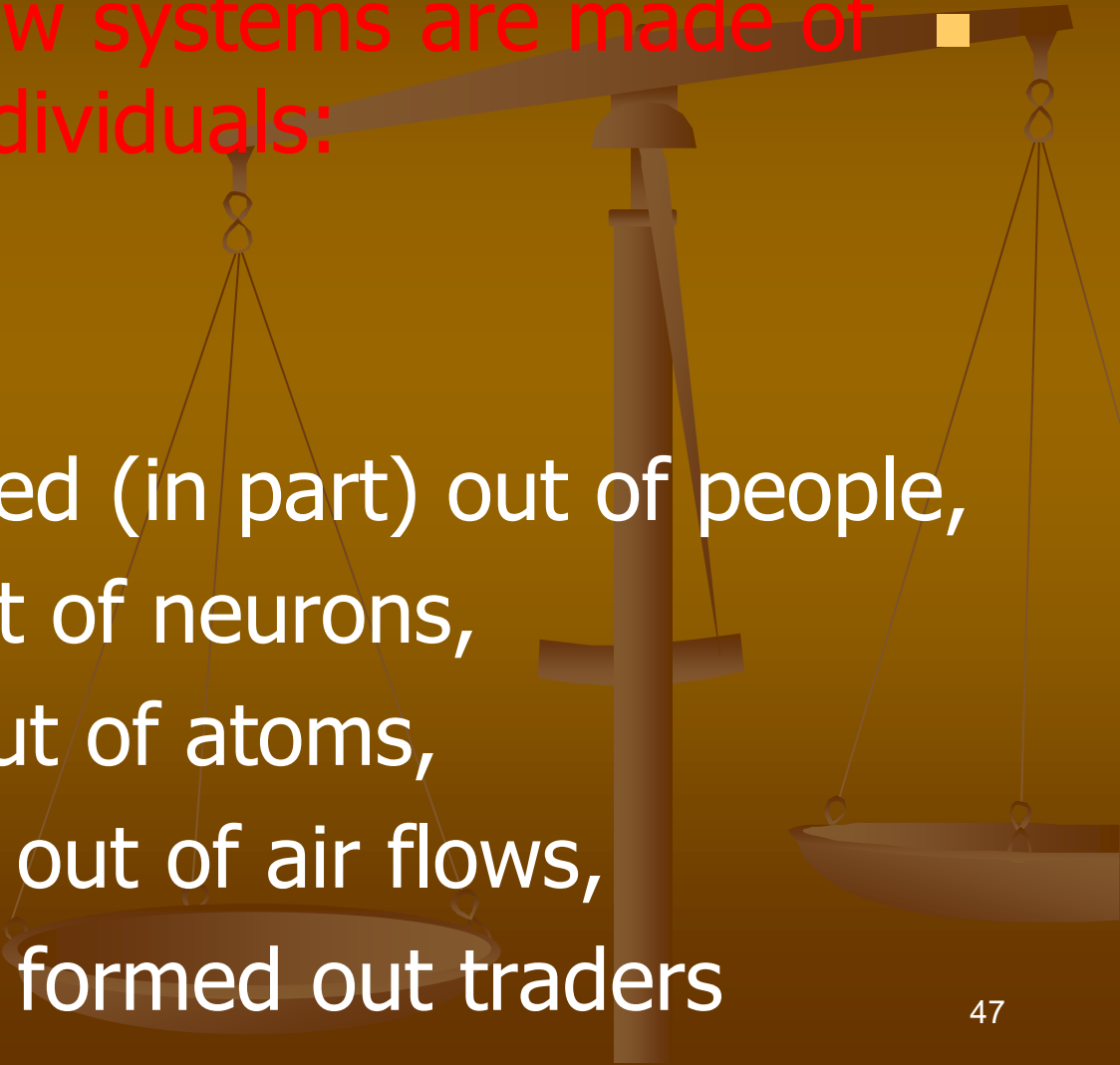
What is A Complex System?

A collection of individuals
whose behavior affects the total in a way which
is unclear to the observer

The parts are interdependent.
So pushing on a complex system "here",
often has effects "over there"

It involves Multi Scale Hierarchies ,

Indeed, the below systems are made of individuals:



Social systems formed (in part) out of people,
the brain formed out of neurons,
molecules formed out of atoms,
the weather formed out of air flows,
the financial market formed out traders

Understanding Complex Systems

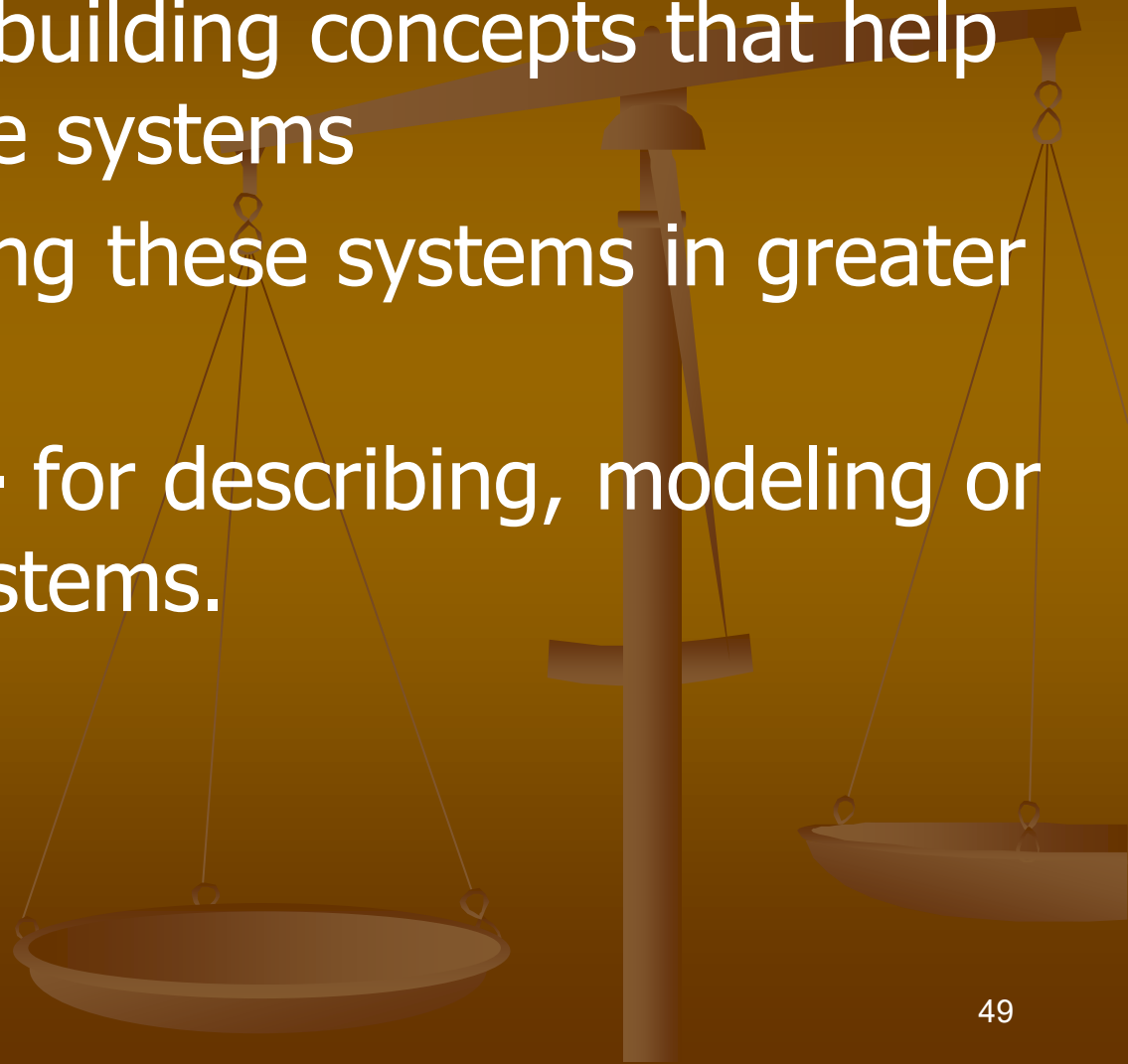
- * **indirect effects.** (causes and effects are not obviously related)
- * how **interactions** give rise to patterns of behavior
- * **how its parts give rise to the collective behavior**
- * how the system **interacts with its environment**
- * their **Multi Scale Hierarchies**
- * the process of formation complex systems through (geometric and algebraic) **pattern formation and evolution** .

Building tools

Conceptual – for building concepts that help us think about these systems

Analytical - studying these systems in greater depth, and

computer based - for describing, modeling or simulating these systems.



In summary

- Cause and affect
- Multi Scale hierarchies
- Interactions
- Evolutions

Are common to all above examples and in particular to the brain and the financial markets

The goal is to transfer methods and discoveries
from Neural Computation to Mathematical Finance

F. Localizing Epileptic Activity

Esther Adi-Japhe
Mina Teicher
Amir Zilberstein
Tomer Gazit

D. Kippervase (Ichilov Hospital)
Miri Neufeld (Ichilov Hospital)
Itzik Fried (Ichilov and UCLA)

Epilepsy is :

- A prevalent neurological disorder
- Characterized by abnormal excessive neuronal activity termed seizures
- An epileptic seizure originates in an epileptic focus located in an epileptic zone
- When medications fail, a surgery is considered in which one needs to locate the epileptic zone
- Surgery is considered when the patient has only one epileptic focus

We produced three accurate Inverse algorithms to localise epileptic focus

If there is an agreement between the EEG raw data and MRI anatomical findings operation can be done

If there is no agreement among the 2 data's then our algorithm will determine, and eliminating the need of a very invasive operation

In this talk we elaborate on one of the Inverse algorithms – the Genetic Algorithm

The inverse algorithms is based on flow measurement and preprocessing

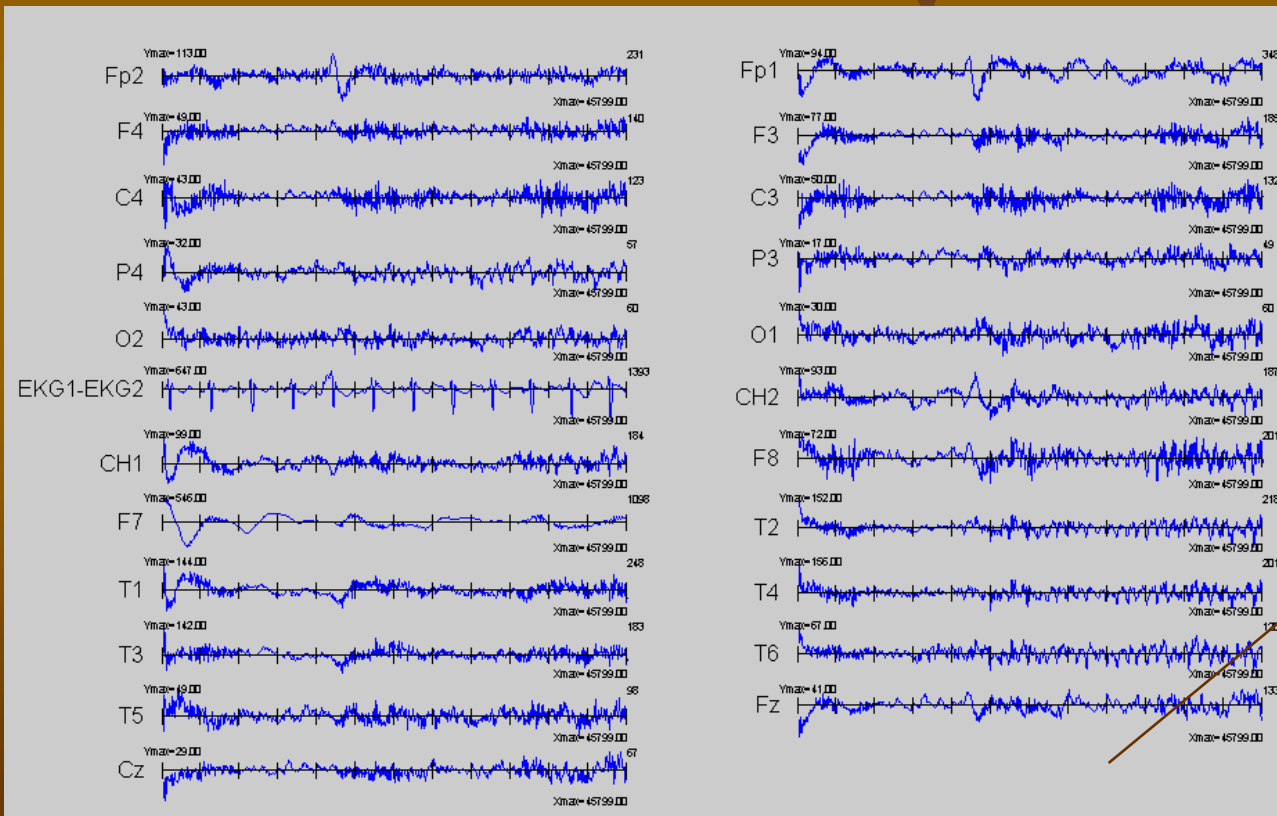
Steps in Localizing the Epileptic zone:

1. Obtain seizure measurements
2. Pre-processing
3. Inverse Algorithm (incl. Brain Model)
4. Compare results with pathology

We are improving almost all parts of the process (especially the green..

1. Obtained seizure measurements

An automatic tools to automatically find a segment of EEG recordings that appears in the beginning of an epileptic activity



2. Preprocessing

- Clean Noise using events contradicting the Dipole fit Model and other methods.
- Calculate the “Amount of Epilepsy” for every electrode (“replacing Amplitude”)
 - The EEG of the event is not characterized by a fixed "shape"
 - Epileptic source can be seen over relatively large time scale

3. INVERSE EEG Algorithm

We look for **N dipoles** which we believe that they formed the EEG measurement for a specific timestamp

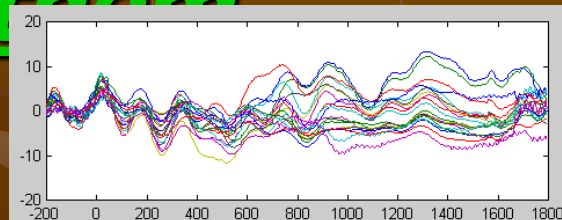
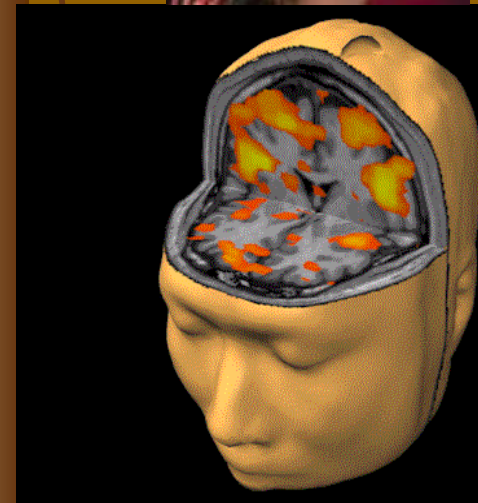
We developed **three algorithmic** approaches for:

- Mapping 3D electrical brain activity
- Finding the location of an interesting phenomena (like epilepsy)

A. **Genetic Algorithm**

B. **Analytic Algorithm**

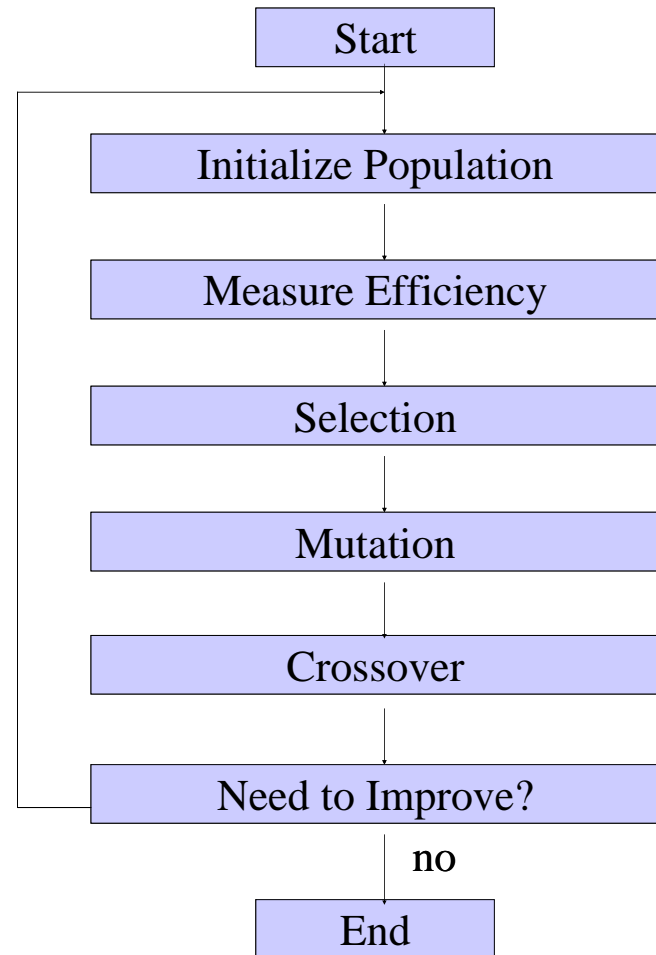
C. **Wavelets**



A. INVERSE EEG Algorithm based on GENETIC Type ALGORITHM

- Genetic algorithms are search algorithms- they are stochastic algorithms, which is a sub-class of Randomized Algorithms
- based on the mechanics of natural selection and natural genetics (Goldberg 1989)
- It consists of 3 steps:
Selection, Crossover, Mutation

Genetic Algorithm- SUMMATION



The adaptation:

1. Our adapted Modification take **time frames of Epilepsy** into account

The solution depends also on:

2. **Measurement properties**

Number of electrodes

Electrodes locations

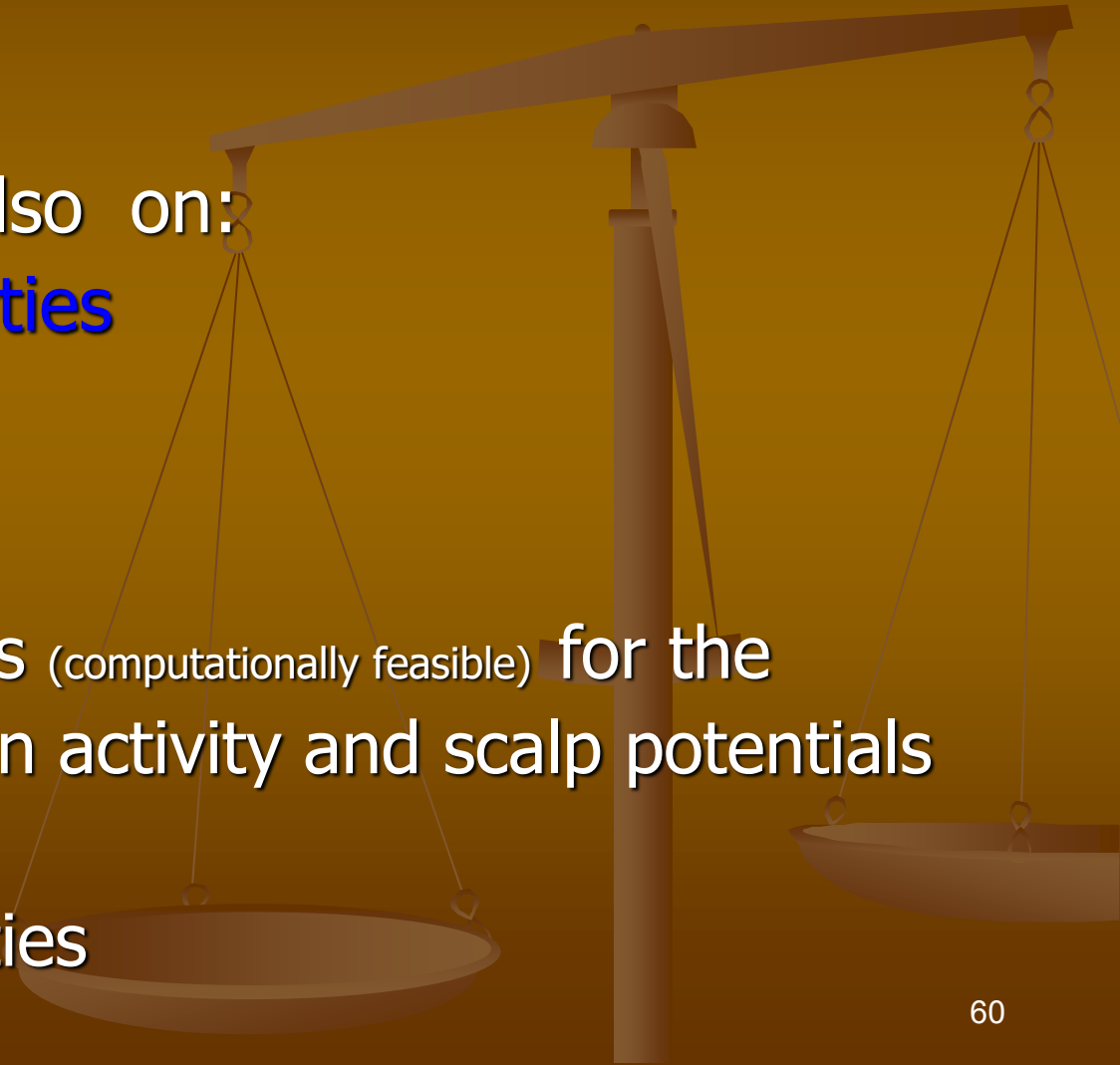
3. **Head model choice**

Find simplified models (computationally feasible) for the relation between brain activity and scalp potentials

4. **Source model choice**

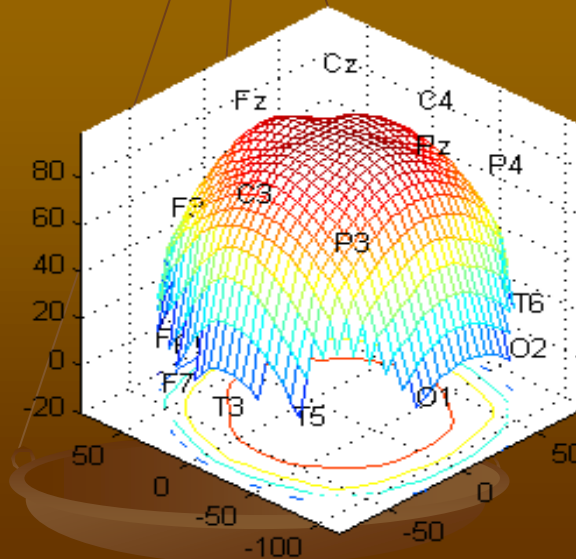
Brain activity properties

5. **Noise**



2. Measurement properties

- Number of electrodes
- Electrodes locations



Central
Frontal
Occipital
Parietal
Temporal

3. Head Models

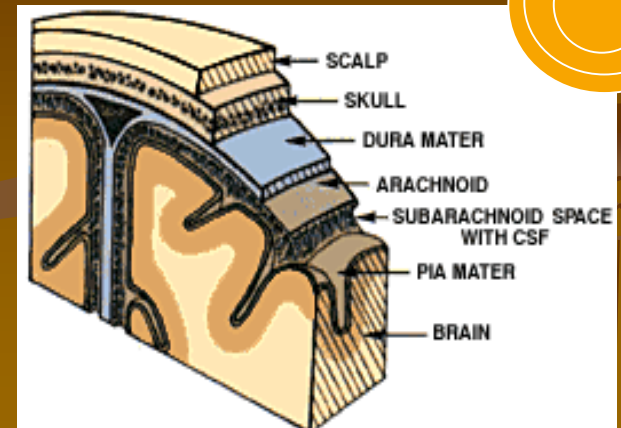
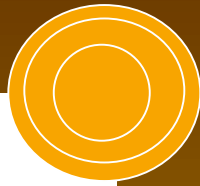
We use 3 types of Head Models for our Forward Computations for EEG

3.1 Layered Head Model

3.2 Realistic Head Models

3.3 Geometric Realistic Head Models

3.1. Layered Head Model



De Munck and Peters 1993

- Properties:
 - Set of concentric spheres
 - Homogeneous conductivity in every layer

Layer	External radius [mm]	Conductivity [S/m]
Scalp	76.49	0.33
Skull	71.76	0.0042
CS fluid	64.03	1.00
Brain	61.53	0.33

*Conductivity and radius measurements from **Ferdjallah 1996**

Layered Head Model

Formula for Potential on the Sculp

$$v(r) = \frac{1}{4\pi} \sum_{j=1}^m (\sigma_j^- - \sigma_j^+) \int_{G_j} J(r') \frac{r - r'}{\|r - r'\|^3} dr'$$

m
 σ_j^-
 σ_j^+

Number of layers

Conductivity inside layer j

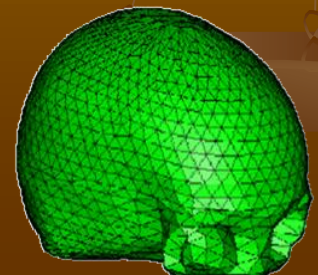
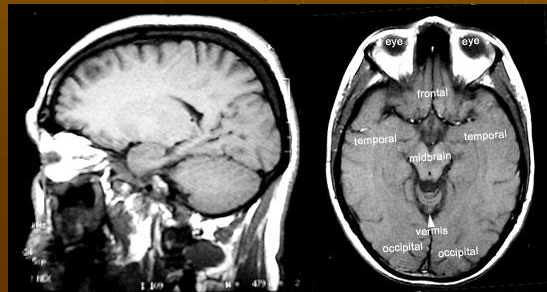
Conductivity outside layer j

■ *Disadvantage of the Layered Head Model :*

Using Perfect Spheres which cannot cover all head areas

3.2. Realistic Head Models (RHM)

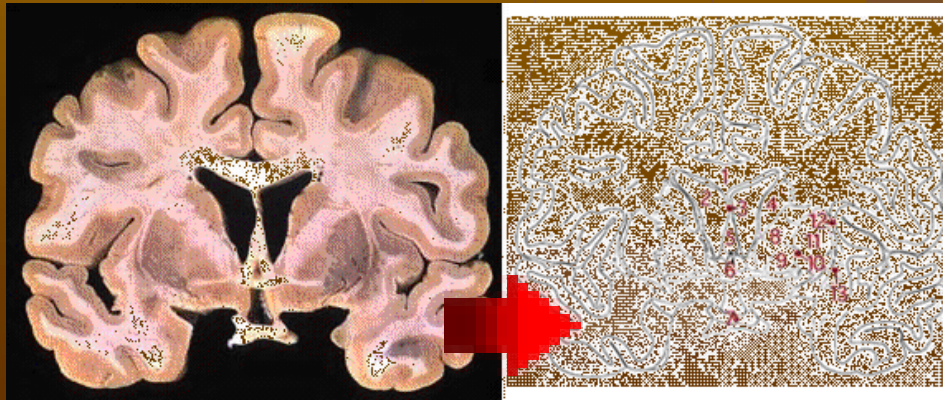
- INPUT: MRI/CT scan (1mm between each cut)
- 2D realization (using differential methods) of the input
- Surface/3D segmentation with equal triangle elements each with its conductivity (equal number of triangles in each layer)
- Interpolation of measured conductivity (between the initial slices)
- Numerical solutions for (Conductivity dependent) Forward Computation (e.g: BEM - Boundary Element Method). (determining potential on the scalp from assumed sources of a specific activity)



3.3. Geometric Realistic Head Model (GRHM)

3D realization of the brain

obtained from the given set of MRI pictures using **Image Processing** (inc **geometrical edge detection**) corresponding to the shape to the internal surfaces.



3.3 Geometric Realistic Head Model (GRHM)

(cont)

Giving

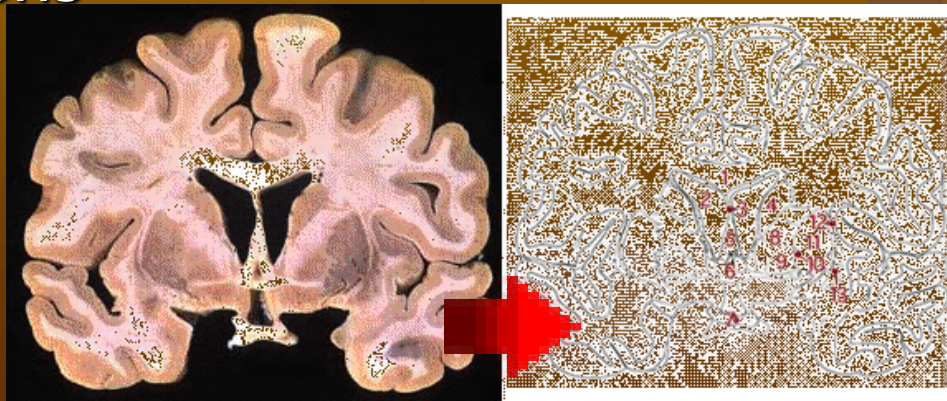
a segmentation

with no equal number of elements in each layer
with different shapes , (not necessarily triangles)

With resolutions which do not depend on other layers.

Advantages:

Resolution Cortex and Dipole Orientation are normal to each other, so we can use this in the model to avoid 'bad' solutions

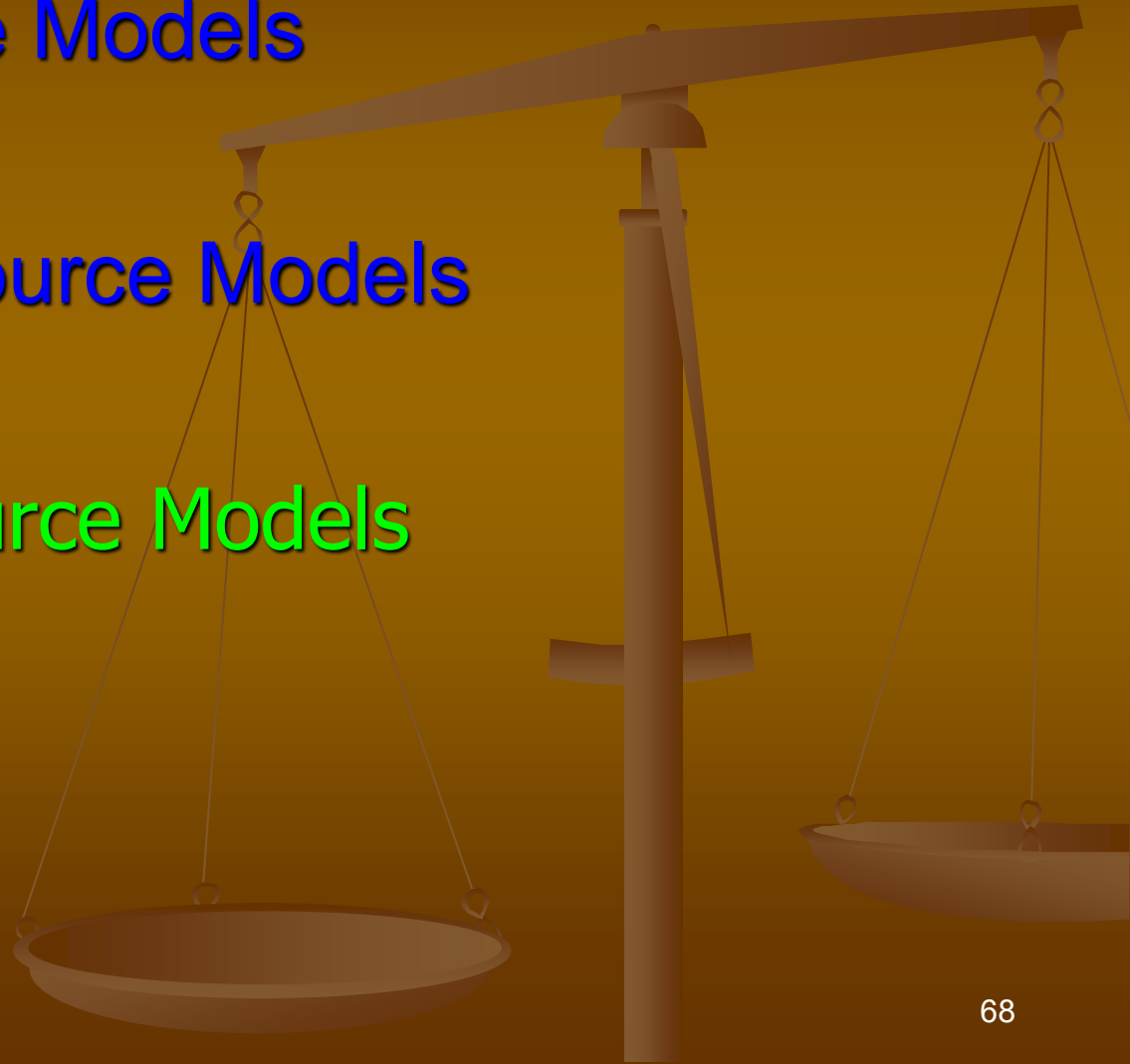


4. Source Models

4.1 Dipole Source Models

4.2 Distributed Source Models

4.3 Improved Source Models



4.1 Dipole Source Models

- Look for the best choice of few dipole(s) position(s) and orientation(s)/amplitudes(s)

Dipole source properties:

- Location: $\mathbf{r}' = (r'_x, r'_y, r'_z)$
- Moment (Orientation) : $\mathbf{J}(\mathbf{r}') = (J_x, J_y, J_z)$

- under search, which is guided by minimization of a cost function - matching the Forward Computations with the input (EEG measurements).

4.2 Distributed Source Models

- Evenly spread fixed locations in the whole brain volume (or on the cortical surface).
- Look for the best choice of amplitudes (and/or orientations) for each location

5.Noise

- Environments noise
- Additive noise on sensors
- Brain background activity
- Physiological (motoric) artifacts

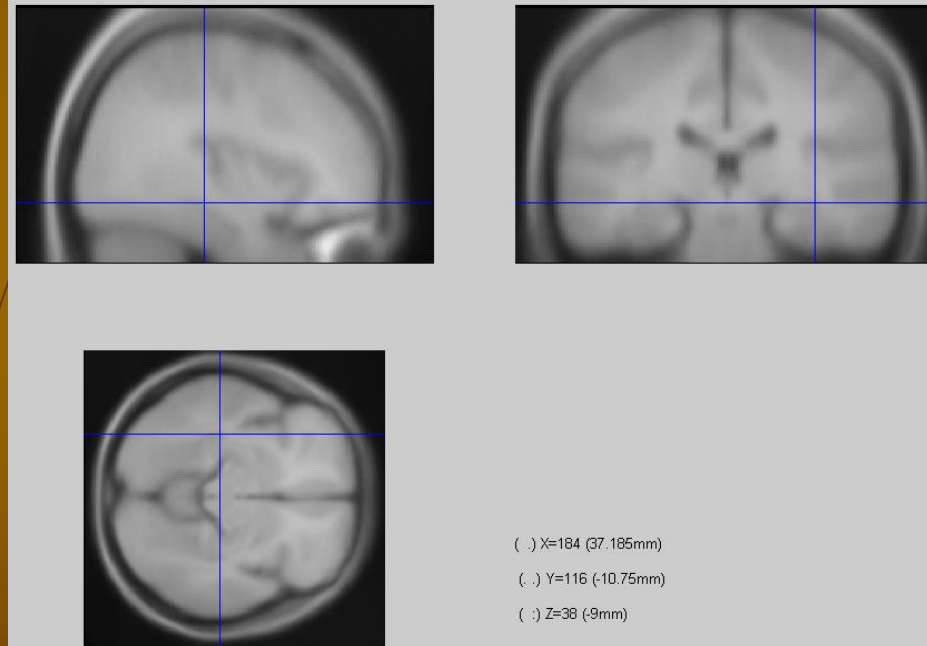


We tested the Genetic Algorithm on simulated data

- Several different head models
- Several different source configurations- simulation
 - Predefined event area/areas
 - Event area/areas activity is simulated using averaged ERP trials
 - Other areas activity is simulated using randomly chosen EEG segments
- Use Forward Computation related to the head model to calculate the electrode 'measurements'
- Add white Gaussian noise to 'measurements'
- Data SNR (Signal to Noise Ratio) is known and can be controlled

Comparing Results (Real Data)

- temporal lobe patients
- Candidates for surgery
- Results were in accordance with pathology



B. Inverse EEG solutions based on Distributed Source Models

Notations

- N_V - # of sources
- J - Vector of source amplitudes
(known locations)
- N_E - # of measurement points
- Φ - Vector of amplitude measurements
(known locations)
- K - Lead Field Matrix determining a linear Forward Computation

Notations - cont

- K is matrix of size $N_V * N_E$
- Example for K:
$$k_{\alpha\beta} = k(r_\alpha, r'_\beta) = \frac{1}{4\pi} \frac{(r_\alpha - r'_\beta)}{\|r_\alpha - r'_\beta\|^3}$$
 (1 layer, conductivity 1)
- For noise free measurements: $\Phi = KJ$

Remark

- Note that since $N_V > N_E$ there is an infinite number of inverse solutions

Existing Inverse EEG solutions based on Distributed Source Models

- MNE - Minimum Norm Estimates (*Hamalainen and Ilmoniemi, 1984*)

Search for the minimum power solution
(minimize the ordinary quadratic L2 norm)

Find J s.t., $\min_J \{ \|\Phi - KJ\|^2 + \lambda \|J\|^2 \}$

The inverse solution is $J = K^T [KK^T + \lambda I]^{-1} \Phi$

- LORETA - Low Resolution Brain Electromagnetic Tomography
(*R.D. Pascual-Marqui et al., 1994*)

Search for the smoothest solution
(minimize the Laplacian of the depth-weighted current distribution)

Improved Distributed Source Methods

- Former distributed source solutions ignore the time domain
- Goal: Force smoothness of sources over time which vanish over polynomials of a given degree.
- **UNDER A PATENT APPLICATION**

The End







One more slide



Speech Recognition

Acoustic Detection of the Red Palm Weevil Based on Speaker Recognition Paradigm



Automatic Acoustic Detection of the Red Palm Weevil,
In "Computers and electronics in Agriculture" 2008

Y. Pinhas, V. Soroker, A. Hetzroni, A. Mizrahi, M. Teicher, I. Goldberger